

# Principles of MRI

EE225E / BIO265

## RF Excitation (Chap. 6)

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- Energy is deposited into the system
- RF pulses used for:
  - Excitation
  - Contrast manipulation
  - Refocussing (...more later)
  - Saturation
  - Tagging
  - Transfer of magnetization

## RF Excitation (Chap. 6)

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- History:
  - 80's - 90's Lots of Research
  - Mid 90's most problems figured out
  - Mid 2000 new burst of research with multiple  
xmitters

## Excitation

- Excitation is short  $\sim 2\text{-}3\text{ms}$ . Can neglect relaxation
- Simplified Block eq

$$\vec{B}_{ROT} = \left( B_0 - \frac{\omega_0}{\gamma} \right) \hat{k}_r + \vec{G} \cdot \vec{x} \hat{k}_r + B_{1,x} \hat{i}_r + B_{1,y} \hat{j}_r$$

And

$$\left( \frac{d\vec{M}}{dt} \right)_{ROT} = -\gamma \vec{B}_{ROT} \times \vec{M}_{ROT}$$

- Only defines rotations!

## Excitation

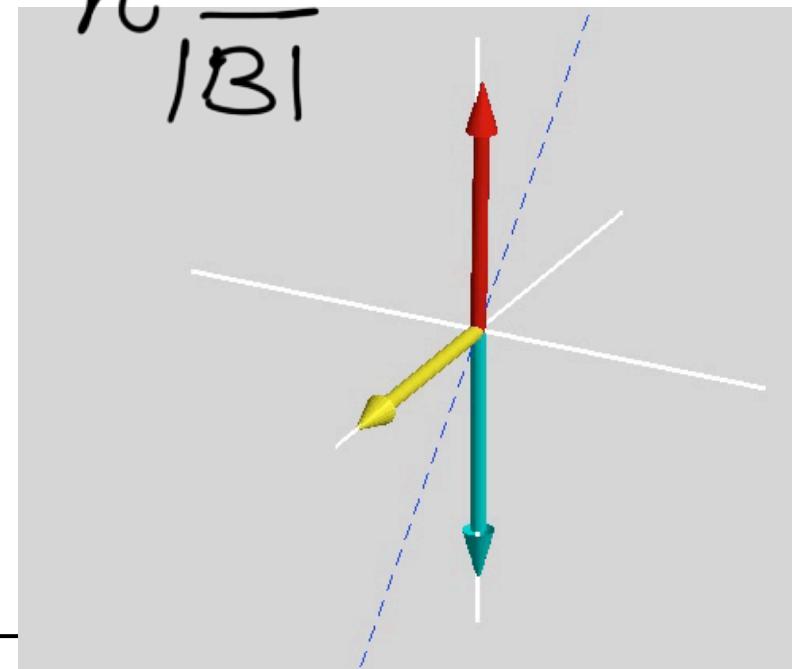
- $\vec{\mu}$  Precesses around  $\vec{B}$
- Frequency of rotation is

$$\omega = \gamma |\vec{B}|$$

- Axis of rotation is

$$\vec{n} \frac{\vec{B}}{|\vec{B}|}$$

normal



## Rotating Frame

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- In rotating frame at  $\omega_0$ ,  $\mathbf{B} + \omega_0/\gamma = 0$

$$\mathbf{B}_{\text{eff}} = [B_{1x}, B_{1y}, \gamma \vec{G} \cdot \vec{r}]^T$$

- Bloch equation for excitation:

$$\begin{bmatrix} \dot{M}_x \\ \dot{M}_y \\ \dot{M}_z \end{bmatrix} = \begin{bmatrix} 0 & \gamma \vec{G} \cdot \vec{r} & -\gamma B_{1y} \\ -\gamma \vec{G} \cdot \vec{r} & 0 & \gamma B_{1x} \\ \gamma B_{1y} & -\gamma B_{1x} & 0 \end{bmatrix} \begin{bmatrix} M_x \\ M_y \\ M_z \end{bmatrix}$$

## RF Excitation

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- Several Special cases:
  - Gradient is on:  $\gamma \vec{G} \cdot \vec{r} \neq 0$   
excitation is spatially selective (next week)
  - Gradient is off:  $\gamma \vec{G} \cdot \vec{r} = 0$   
non-selective excitation (Today)

## Non Selective Excitation

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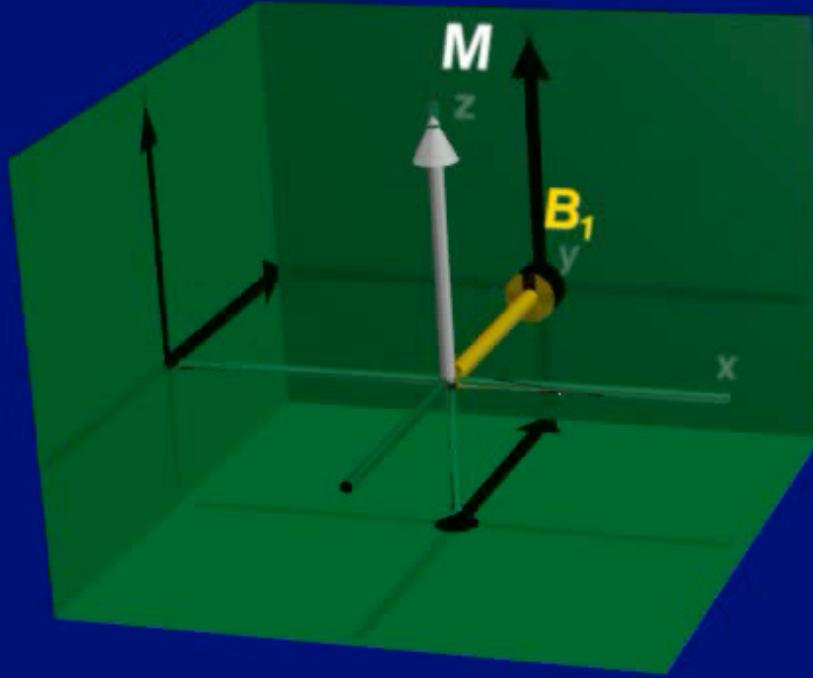
$$\begin{bmatrix} \dot{M}_x \\ \dot{M}_y \\ \dot{M}_z \end{bmatrix} = \begin{bmatrix} 0 & 0 & -\gamma B_{1y} \\ 0 & 0 & \gamma B_{1x} \\ \gamma B_{1y} & -\gamma B_{1x} & 0 \end{bmatrix} \begin{bmatrix} M_x \\ M_y \\ M_z \end{bmatrix}$$

$$B_{\text{eff}} = [B_{1x}, B_{1y}, 0]^T$$

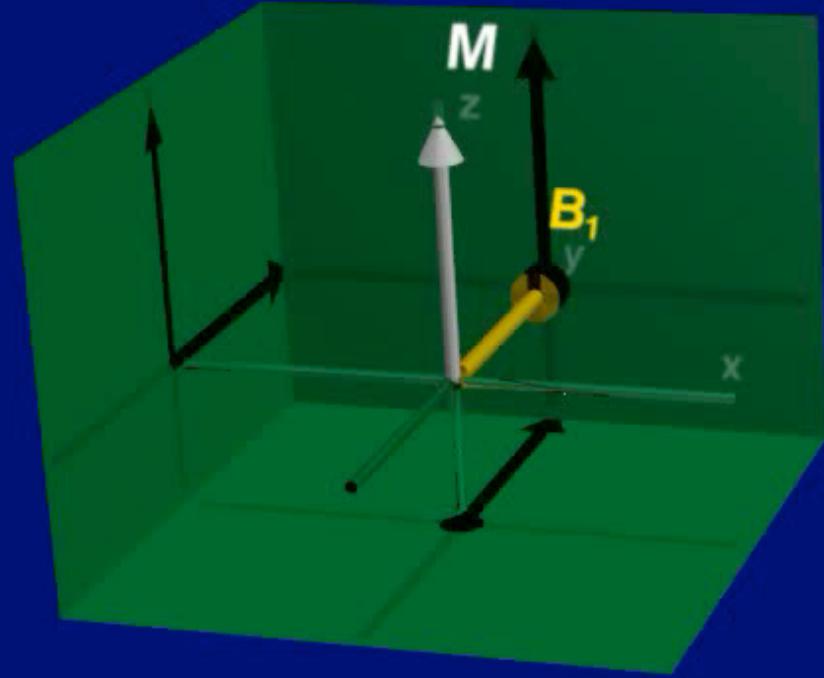
- Magnetization precesses around  $B_{\text{eff}}$

# RF Excitation

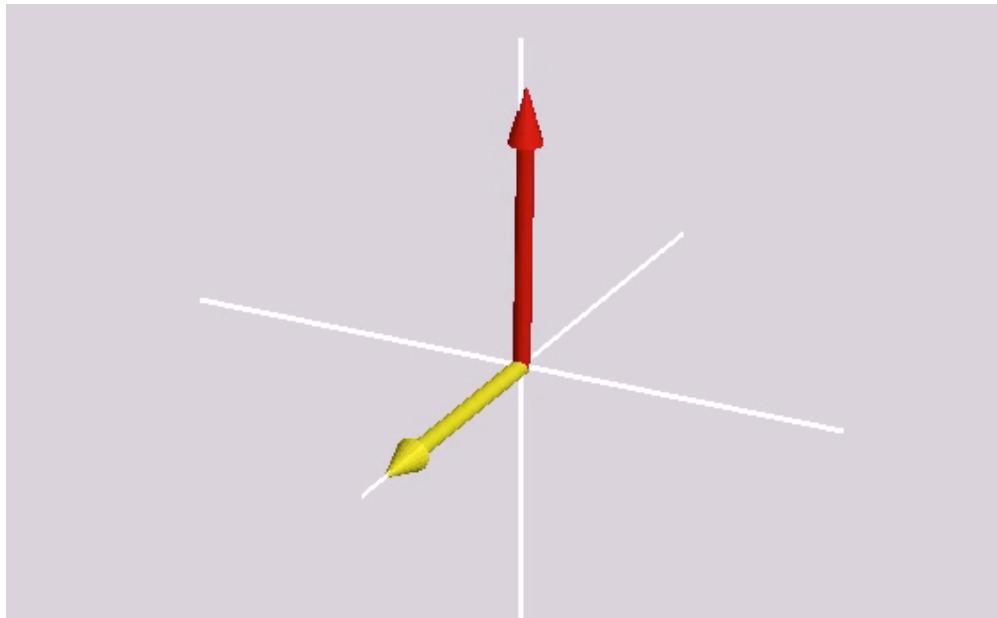
Lab Frame



Rotating Frame



# RF Excitation



$$\vec{B}_{\text{eff}} = (B_{1,z}, 0, 0)$$

$$\vec{n} = (1, 0, 0)$$

$$\omega_r = \gamma B_{1,z}$$

$\vec{M}$  ROTATES IN

Z-Y PLANE.

If  $B_{1,y}$  is constant

RF



ANGLE OF ROTATION IS

$$\Theta = \gamma B_{1,z} \gamma$$

## Time Varying B1

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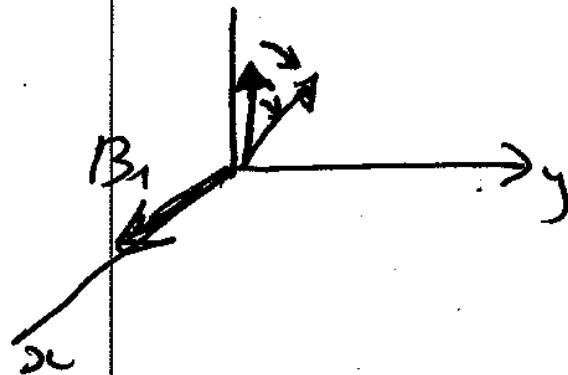
- For time varying B1:

$$\theta = \gamma \int_0^t B_{1x}(\tau) d\tau$$

- Rotations about a common axis add!  
(not true in general)

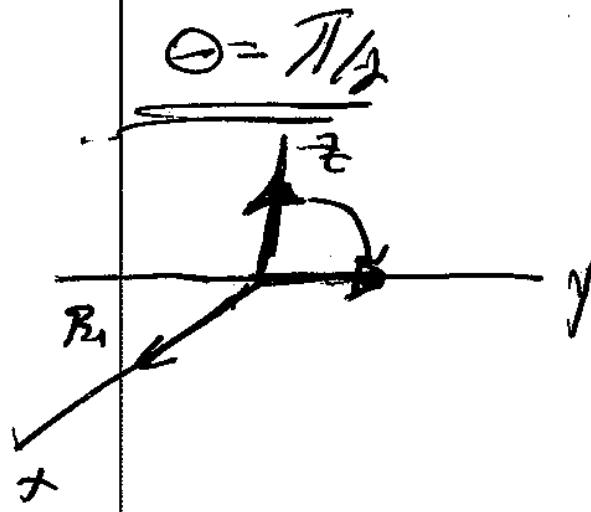
# Useful Rotations

$$0 < \theta < \frac{\pi}{2}$$



SMALL TIP-ANGLE EXCITATION

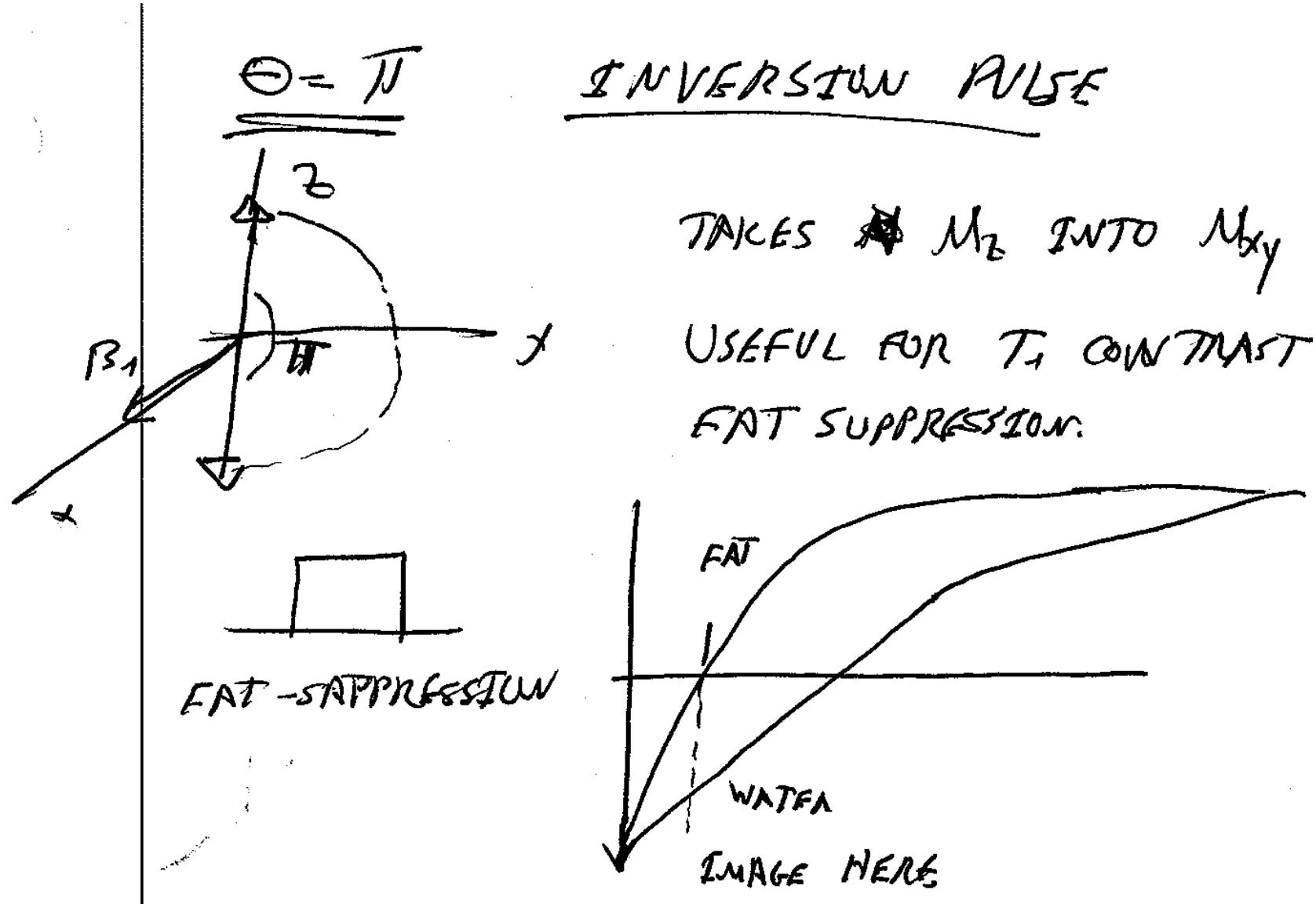
CREATES SOME  $M_{x,y}$   
LEAVES SOME  $M_z$   
USEFUL FOR FAST IMAGING.



EXCITATION PULSE

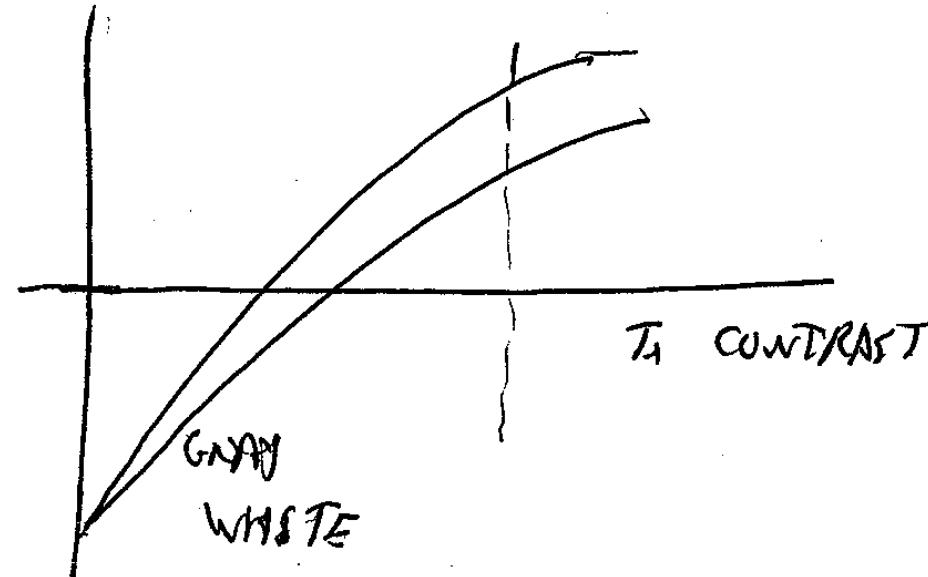
TAKES  $M_z$  INTO  $M_{x,y}$   
MAX SIGNAL  
NO  $M_z$  LEFT!

# Useful Rotations

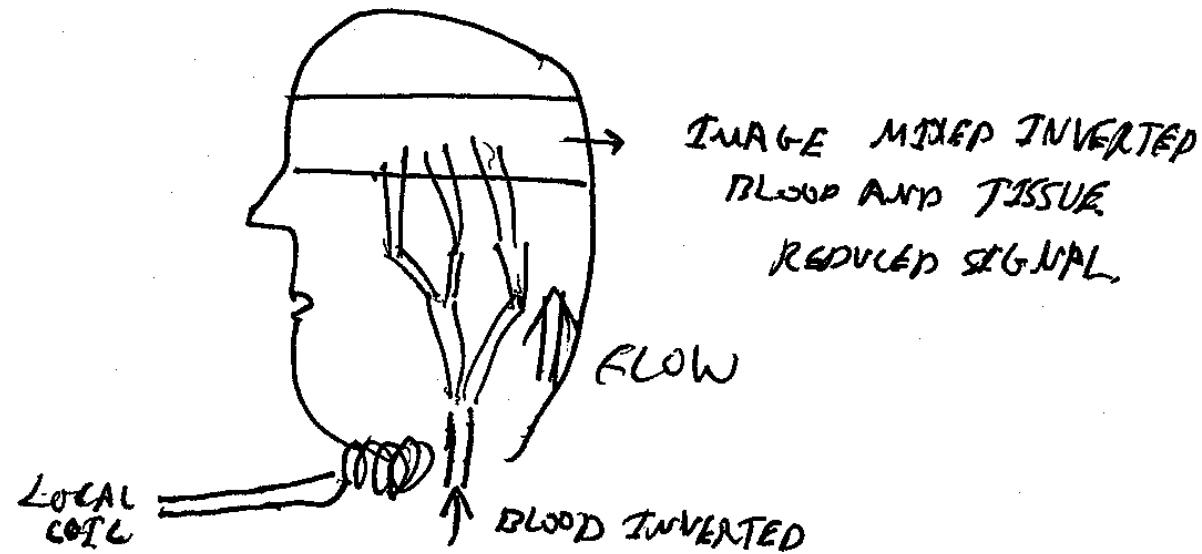


# Useful Rotations

$T_1$  CONTRAST

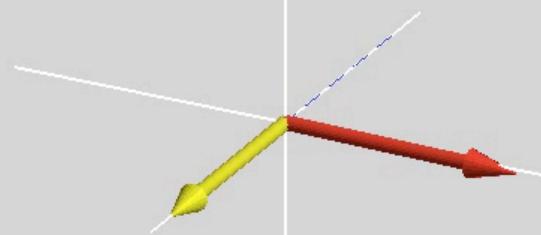


ASL

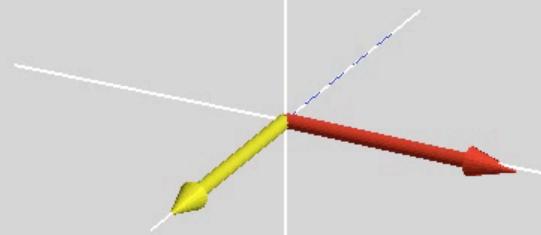


# What do these pulses do?

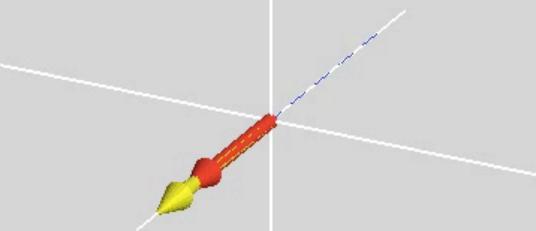
$$\theta = \frac{\pi}{2}$$



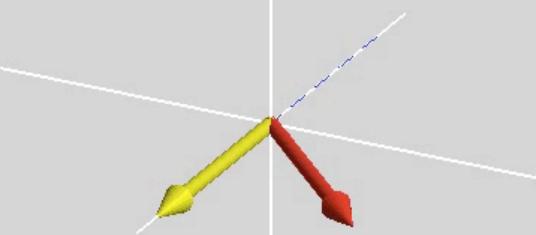
$$\theta = \pi$$



$$\theta = \pi$$



$$\theta = \pi$$

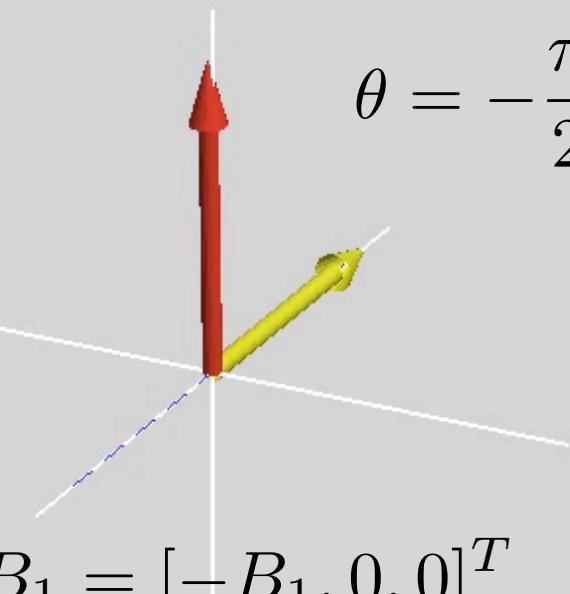


## Example: Non selective RF

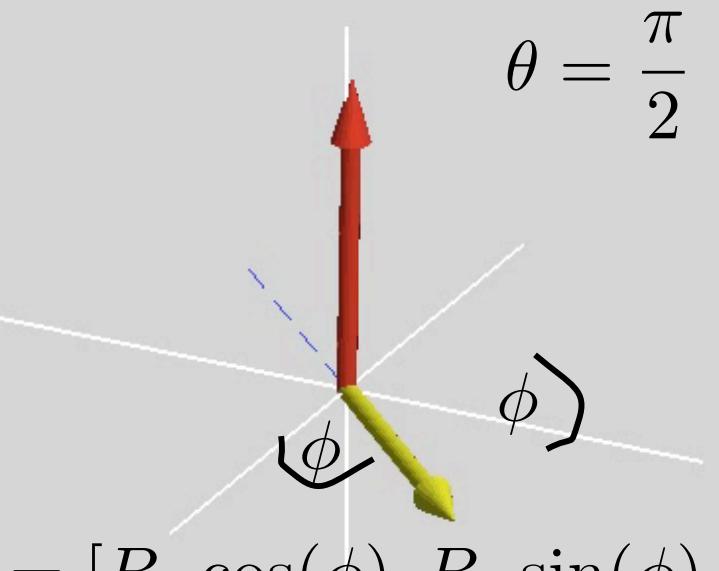
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- Typical Numbers:
  - $B_1 = 0.1\text{G}$
  - $\omega_1 = \gamma B_1 = 2\pi 425.7 \text{ rad/sec}$
  - $f_1 \approx 426\text{Hz}$
- For a  $\pi/2$  pulse: 1/4 rotation
  - $\tau \approx 1000/426 * 1/4 = 0.6 \text{ ms}$

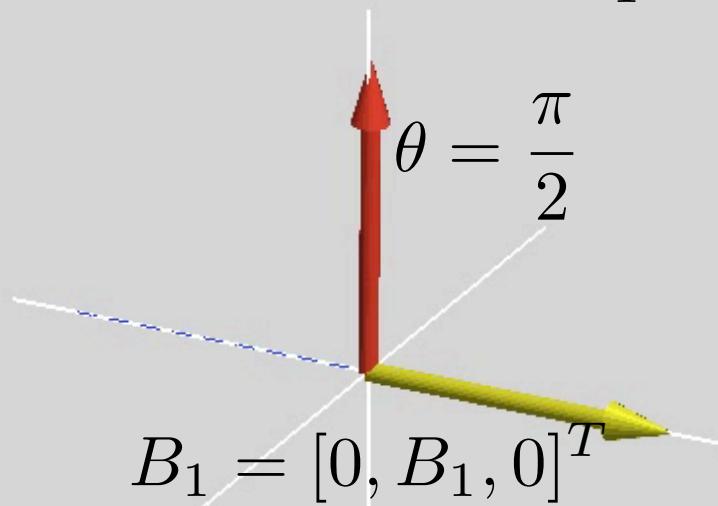
# What do these pulses do?


$$\theta = -\frac{\pi}{2}$$

$$B_1 = [-B_1, 0, 0]^T$$


$$\theta = \frac{\pi}{2}$$

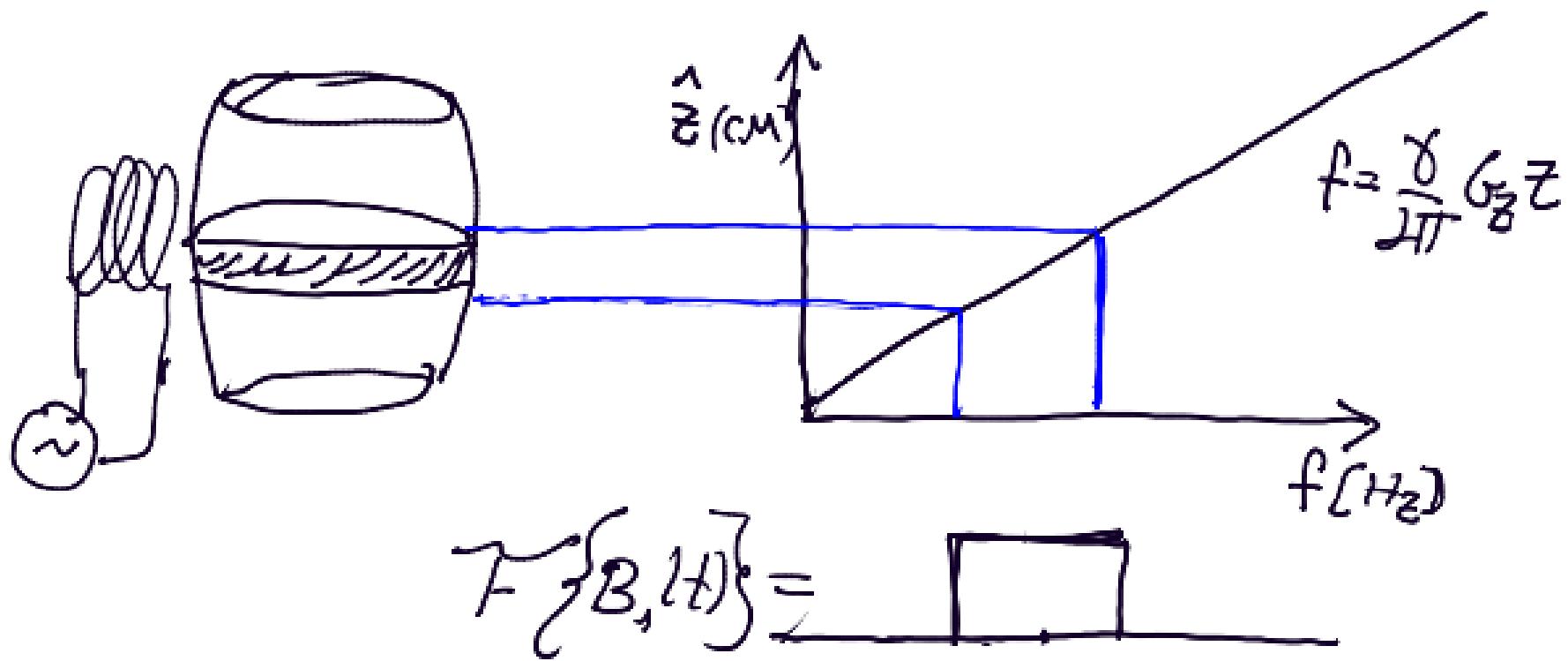
$$B_1 = [B_1 \cos(\phi), B_1 \sin(\phi), 0]^T$$


$$\theta = \frac{\pi}{2}$$

$$B_1 = [0, B_1, 0]^T$$

## Slice Selective Example

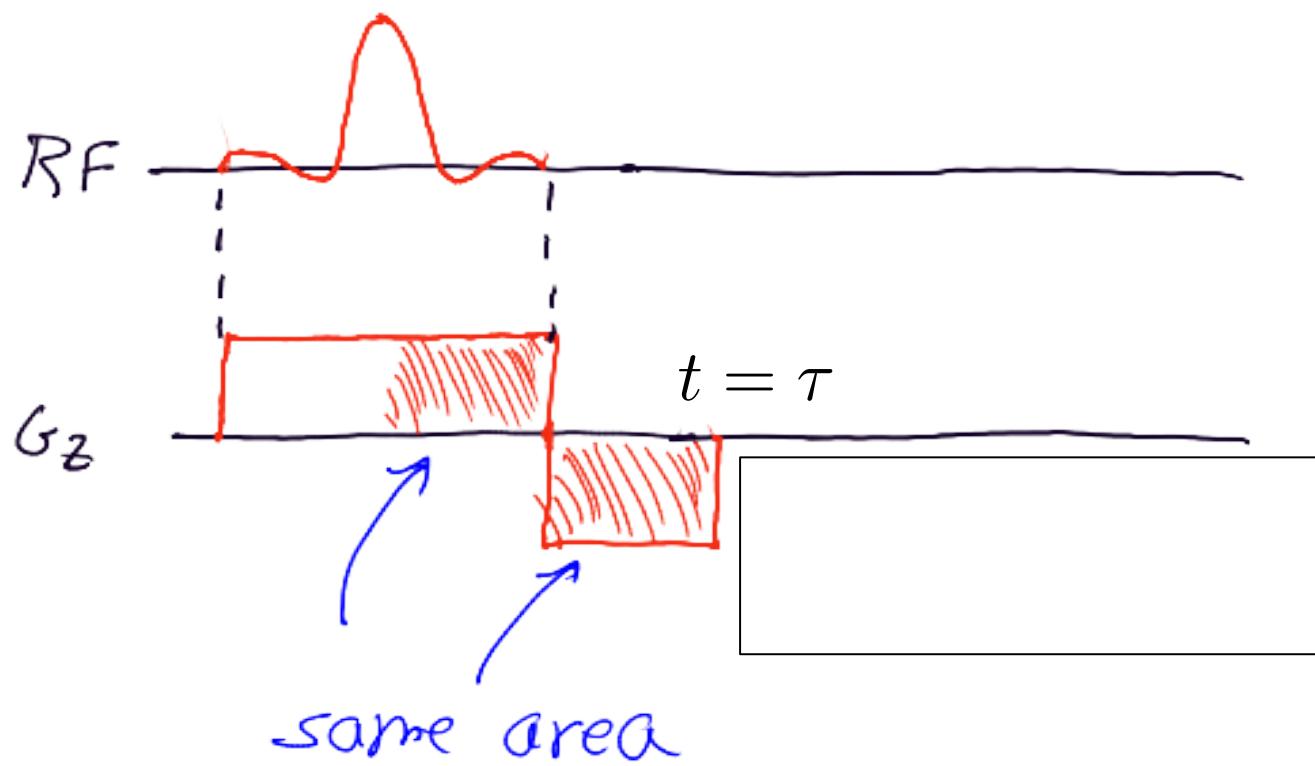
$$\vec{G} = [0, 0, \vec{G}_z]^T$$



Only spins near resonance frequency are excited.

# Slice Selective Example

pulse sequence:

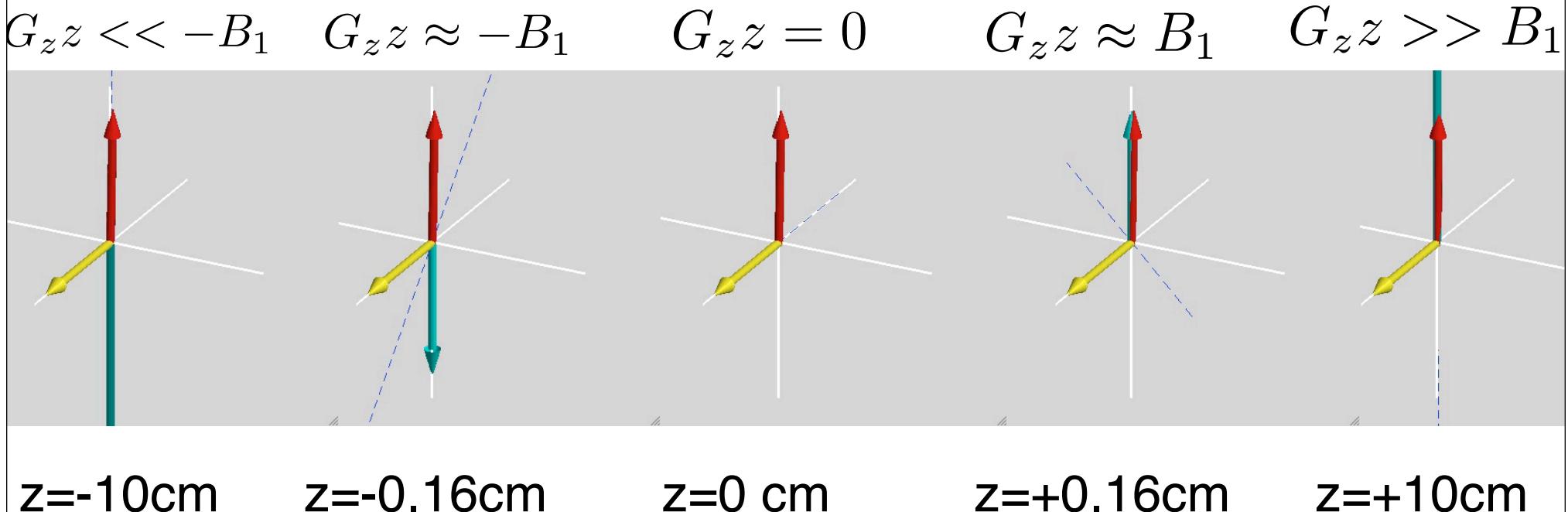


Q: What is:  $M_{xy}(\vec{r}, \tau)$  ?

## Slice Selectivity as Rotations

- $B_{1x}, B_{1y}$  are the same **EVERWHERE**
- $G_z z$  changes linearly with  $z$

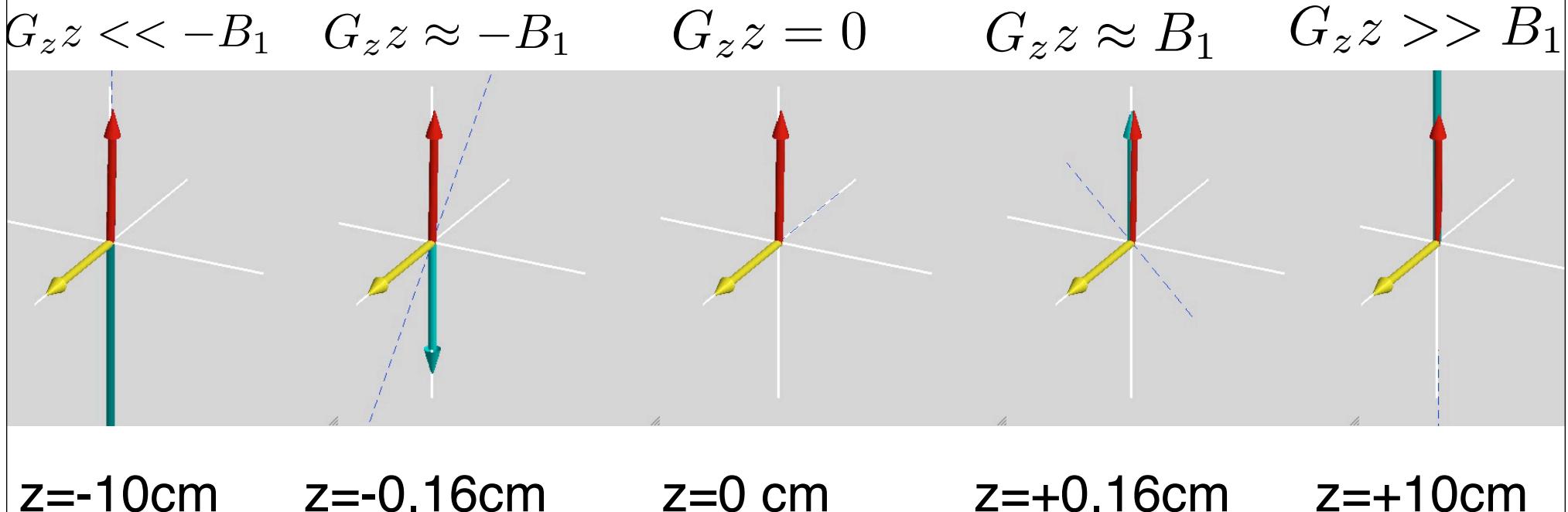
Example:  $G_z = 1 \text{ G/cm}$ ,  $B_{1x} = 0.16 \text{ G}$ :



## Slice Selectivity as Rotations

- $B_{1x}, B_{1y}$  are the same **EVERWHERE**
- $G_z z$  changes linearly with  $z$

Example:  $G_z = 1 \text{ G/cm}$ ,  $B_{1x} = 0.16 \text{ G}$ :



## Slice Selectivity

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- Simple Cases:
  - On-Resonance  $\Rightarrow$  same as Non-Selective

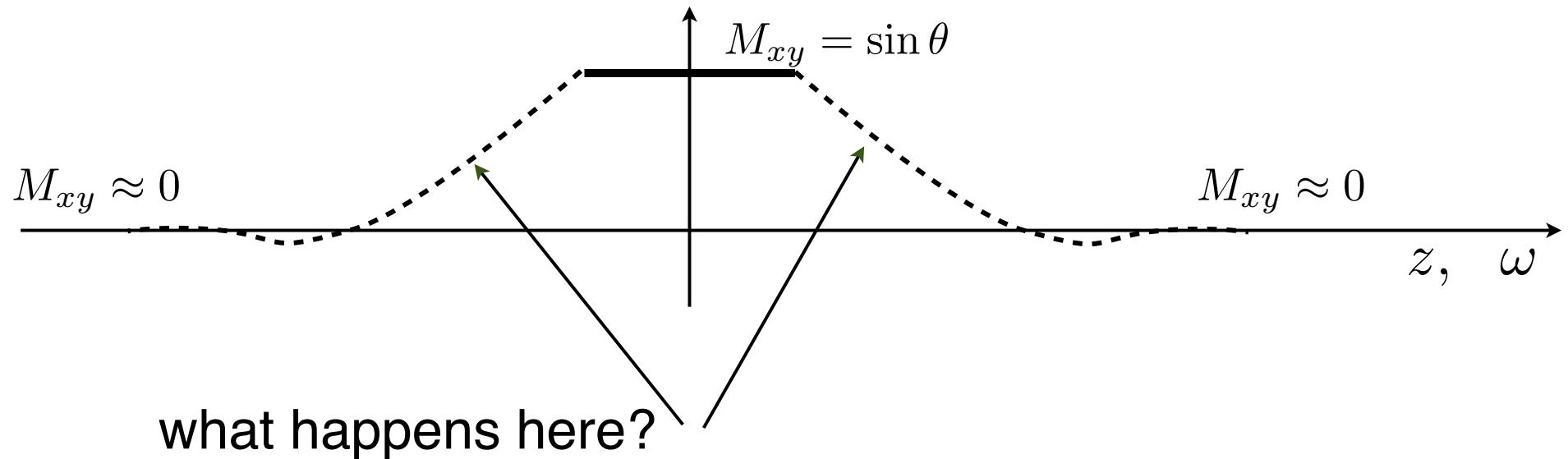
$$G_z z = 0 \Rightarrow \theta = \gamma \int_0^\tau B_1(t) dt$$

- Far off resonance,  $G_z z$  dominates

$$\gamma |G_z z| \gg |B_1| \Rightarrow \vec{n} \approx [0, 0, 1]$$

no  $M_{xy}$  produced!

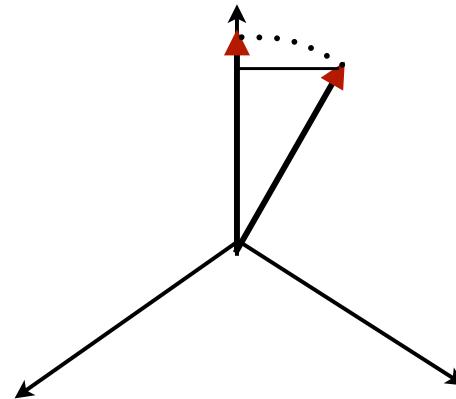
# Slice Selectivity



- In general, a hard problem
  - Rotations  $\Rightarrow$  fundamentally non-linear
- Many Solutions for special cases
  - Including most interesting ones

## Small Tip-Angle Excitation Pulses

- Basic idea:
  - Tip angle is small
  - $M_z \approx M_0$  throughout the excitation pulse



$$M_z = \cos(\theta)M_0 \approx M_0$$

$$M_{xy} = \sin(\theta)M_0 \approx \theta M_0$$

## Bloch Equation - Selective RF

$$\begin{bmatrix} \dot{M}_x \\ \dot{M}_y \\ \dot{M}_z \end{bmatrix} = \begin{bmatrix} 0 & \gamma \vec{G} \cdot \vec{r} & -\gamma B_{1y} \\ -\gamma \vec{G} \cdot \vec{r} & 0 & \gamma B_{1x} \\ \gamma B_{1y} & -\gamma B_{1x} & 0 \end{bmatrix} \begin{bmatrix} M_x \\ M_y \\ M_z \end{bmatrix}$$

If  $M_z \approx M_0$  the last equation decouples!

$$\begin{bmatrix} \dot{M}_x \\ \dot{M}_y \\ \dot{M}_z \end{bmatrix} = \begin{bmatrix} 0 & \gamma \vec{G} \cdot \vec{r} & -\gamma B_{1y} \\ -\gamma \vec{G} \cdot \vec{r} & 0 & \gamma B_{1x} \\ 0 & 0 & 0 \end{bmatrix} \begin{bmatrix} M_x \\ M_y \\ M_z \end{bmatrix}$$

## Bloch Equation - Small Tip Approximation

$$\begin{bmatrix} \dot{M}_x \\ \dot{M}_y \end{bmatrix} = \begin{bmatrix} 0 & \gamma \vec{G} \cdot \vec{r} & -\gamma B_{1y} \\ -\gamma \vec{G} \cdot \vec{r} & 0 & \gamma B_{1x} \end{bmatrix} \begin{bmatrix} M_x \\ M_y \\ M_0 \end{bmatrix}$$

Bloch Eq. Simplifies to:

$$\begin{bmatrix} \dot{M}_x \\ \dot{M}_y \end{bmatrix} = \begin{bmatrix} 0 & \gamma \vec{G} \vec{r} \\ -\gamma \vec{G} \vec{r} & 0 \end{bmatrix} \begin{bmatrix} M_x \\ M_y \end{bmatrix} + \begin{bmatrix} -\gamma B_{1y} \\ \gamma B_{1x} \end{bmatrix} M_0$$

Precession  
(like reception)    Excitation

Note: M<sub>x</sub>, M<sub>y</sub>, G, B<sub>1</sub> are a function of time!

## Small Tip-Angle Approximation

- Example: ISO-Center  $B_1=B_{1x}$

$$\begin{bmatrix} \dot{M}_x \\ \dot{M}_y \end{bmatrix} = \begin{bmatrix} 0 \\ \gamma B_{1x} \end{bmatrix} M_0$$

- $M_{xy} = M_x + iM_y$  is linear with  $B_1$  !

$$M_{xy} = i\gamma B_{1x} M_0 t$$

## Derivation

$$\begin{bmatrix} \dot{M}_x \\ \dot{M}_y \end{bmatrix} = \begin{bmatrix} 0 & \gamma \vec{G} \cdot \vec{r} \\ -\gamma \vec{G} \cdot \vec{r} & 0 \end{bmatrix} \begin{bmatrix} M_x \\ M_y \end{bmatrix} + \begin{bmatrix} -\gamma B_{1y} \\ \gamma B_{1x} \end{bmatrix} M_0$$

$$\begin{aligned} \dot{M}_x + i \dot{M}_y &= -i \gamma \vec{G} \cdot \vec{r} M_y - i \gamma \vec{G} \cdot \vec{r} M_x - \\ &\quad (-i \gamma B_{1y} + i \gamma B_{1x}) M_0 \\ &= (-i \gamma \vec{G} \cdot \vec{r})(\underbrace{M_x + i M_y}_{M_{xy}}) + i (\underbrace{\gamma B_{1x} + i \gamma B_{1y}}_{\gamma B_1}) M_0 \end{aligned}$$

## Derivation

$$M_{xy} = (-i\gamma \vec{G} \cdot \vec{r}) M_{xy} + i\gamma B_1 M_o$$

- Solve like in the reception case!

- Integrating factor:

$$e^{i \int_{-\infty}^t \gamma \vec{G} \cdot \vec{r} d\tau}$$

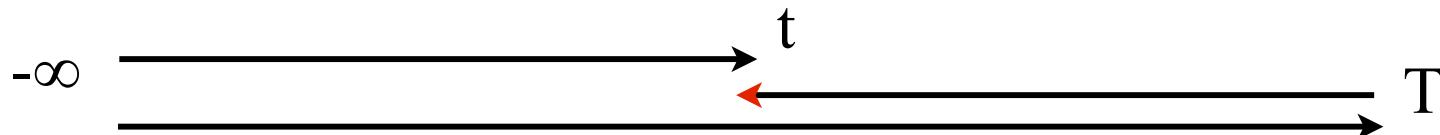
$$\frac{d}{dt} [M_{xy}(\vec{r}, t) e^{i \int_{-\infty}^t \gamma \vec{G} \cdot \vec{r} d\tau}] = i\gamma B_1(t) M_o e^{i \int_{-\infty}^t \gamma \vec{G} \cdot \vec{r} d\tau}$$

## Derivation

- Integrate from  $-\infty$  to  $t=T$  to find  $M_{xy}(r, T)$

$$M_{xy}(\vec{r}, T) \cdot e^{i \int_{-\infty}^T \vec{y} \vec{G}(\tau) \cdot \vec{r} d\tau} = \int_{-\infty}^T i M_0 \gamma B_1(t) e^{i \int_{-\infty}^t \vec{y} \vec{G}(\tau) \cdot \vec{r} d\tau} dt$$

$$M_{xy}(\vec{r}, T) = \int_{-\infty}^T i M_0 \gamma B_1(t) e^{i \int_{-\infty}^t \vec{y} \vec{G}(\tau) \cdot \vec{r} d\tau - i \int_{-\infty}^T \vec{y} \vec{G}(\tau) \vec{r} d\tau} dt$$



## Derivation

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$$M_{xy}(\vec{r}, \tau) = i M_0 \int_{-\infty}^T \gamma B_1(t) e^{-i \int_{\tau}^T \vec{\gamma} \vec{G}(\tau) \cdot \vec{r} d\tau} dt$$

## Small Tip-Angle Approximation

- Solution for general Eq. at time t=T

$$M_{xy}(\vec{r}, T) = iM_0 \int_{-\infty}^T \gamma B_1(t) e^{-i2\pi \vec{k}(t) \cdot \vec{r}} dt$$

, where

$$\vec{k}(t) = \frac{\gamma}{2\pi} \int_t^T \vec{G}(\tau) d\tau$$

- k(t) is area of the remaining gradient

## Example: Slice Selection

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$$M_{xy}(z, T) = iM_0 \int_0^T \gamma B_1(t) e^{-i2\pi k_z(t)z} dt$$

- This is not exactly a Fourier transform
- Would like:

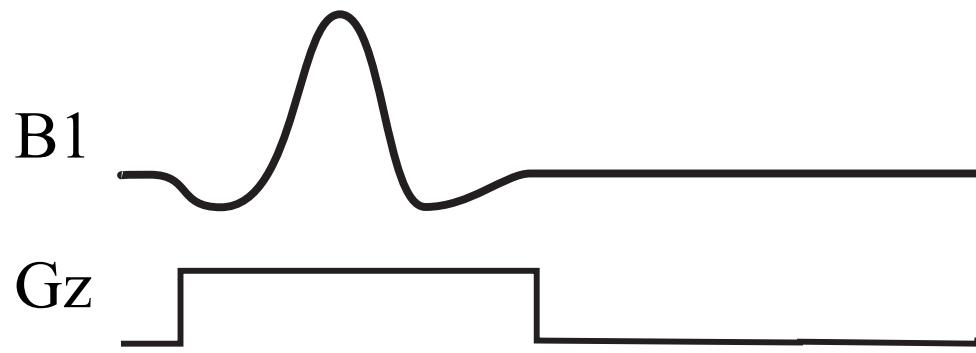
$$M_{xy}(z, T) = iM_0 \int_K W(k) e^{-i2\pi k_z z} dk_z$$

$$W(k) = \frac{2\pi B_1(k)}{|G(k)|}$$

## Example: Slice Selection

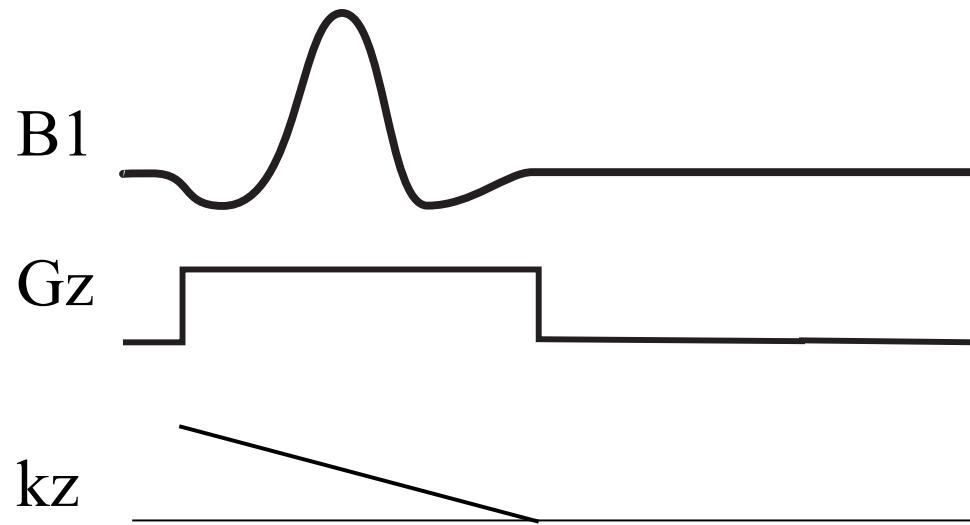
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$$M_{xy}(z, T) = iM_0 \int_0^T \gamma B_1(t) e^{-i2\pi k_z(t)z} dt$$

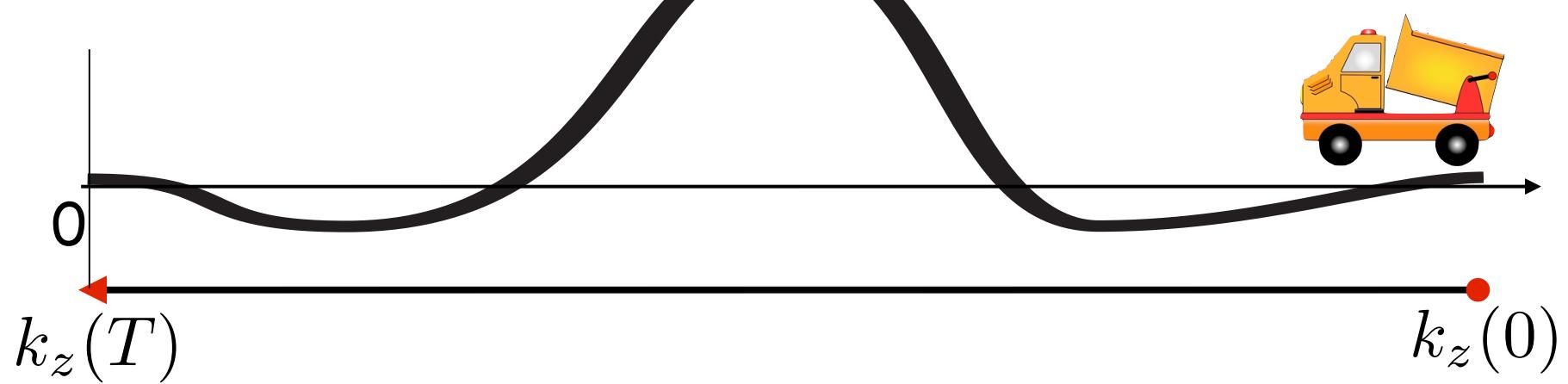


- First find  $k_z(t)$
- Map  $B_1(t)$  to  $k_z(t)$
- Compute the integral (Fourier transform)

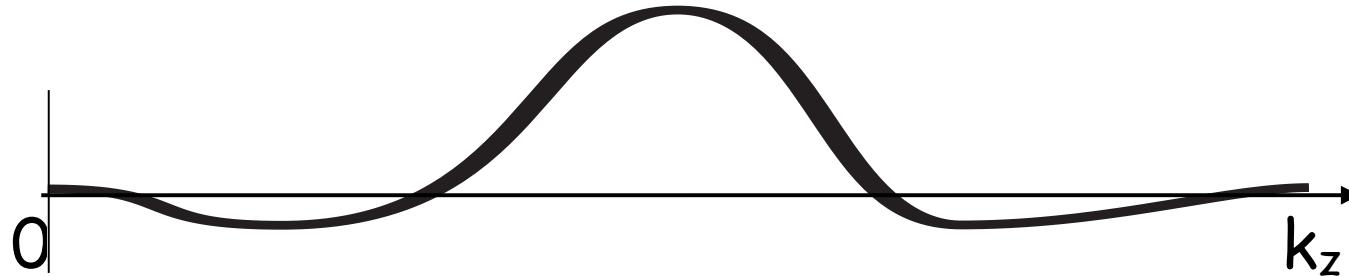
## Example: Slice Selection



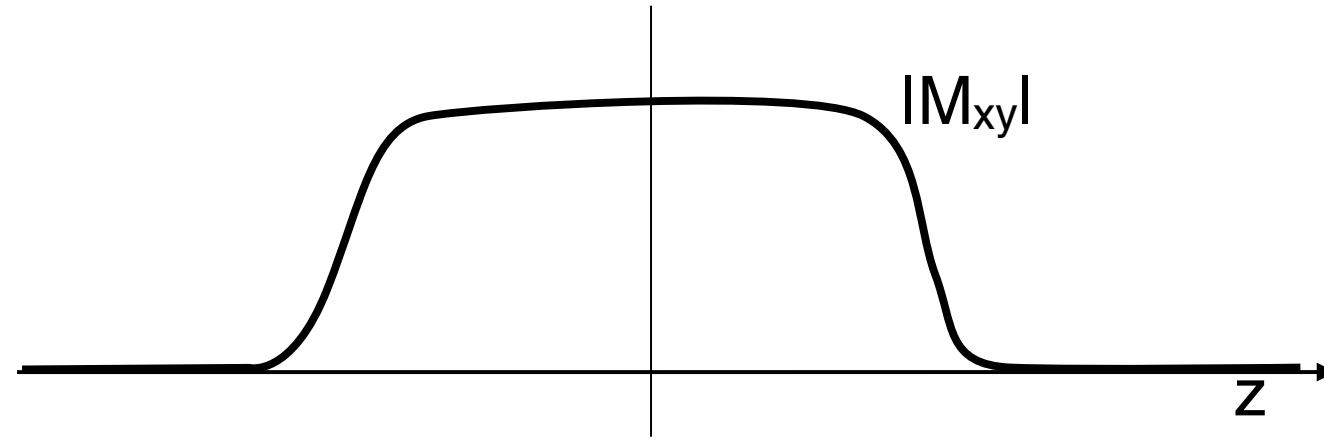
- Plot  $B_1(t)$  vs  $k_z(t)$ :



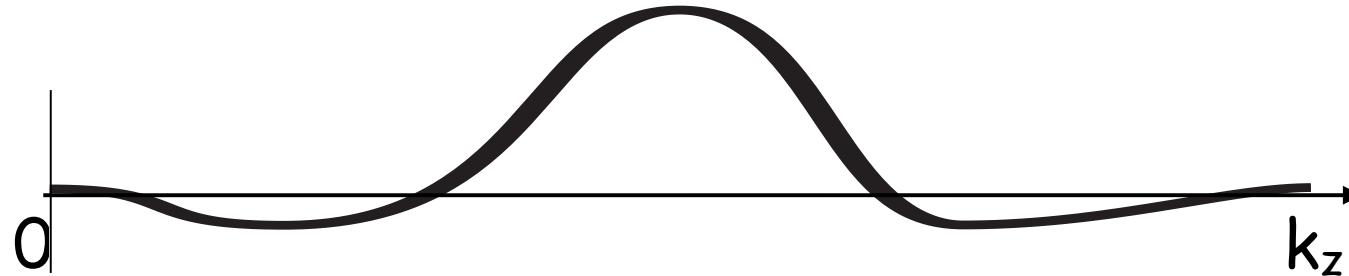
## Example: Slice Selection



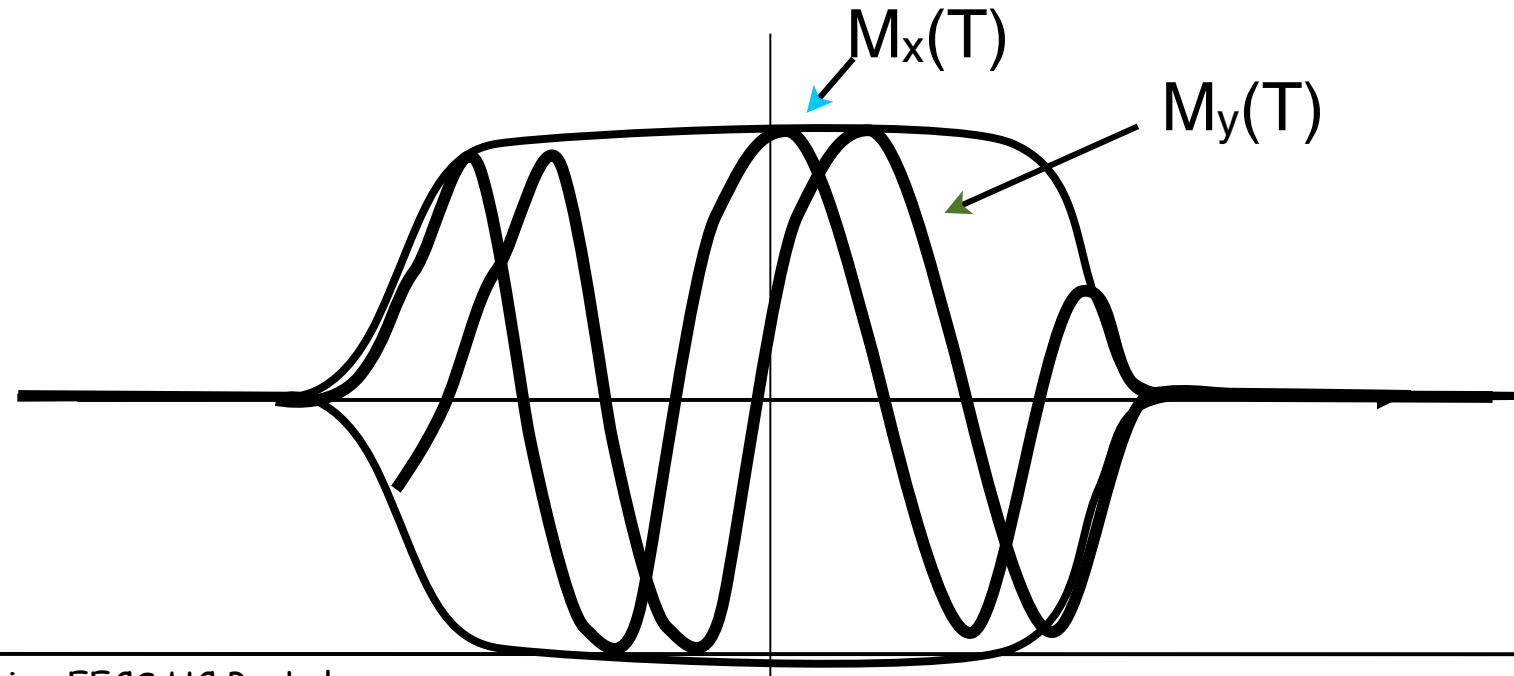
- $B_1$  is not centered in k-space
- We get the right magnitude  $M_{xy}$



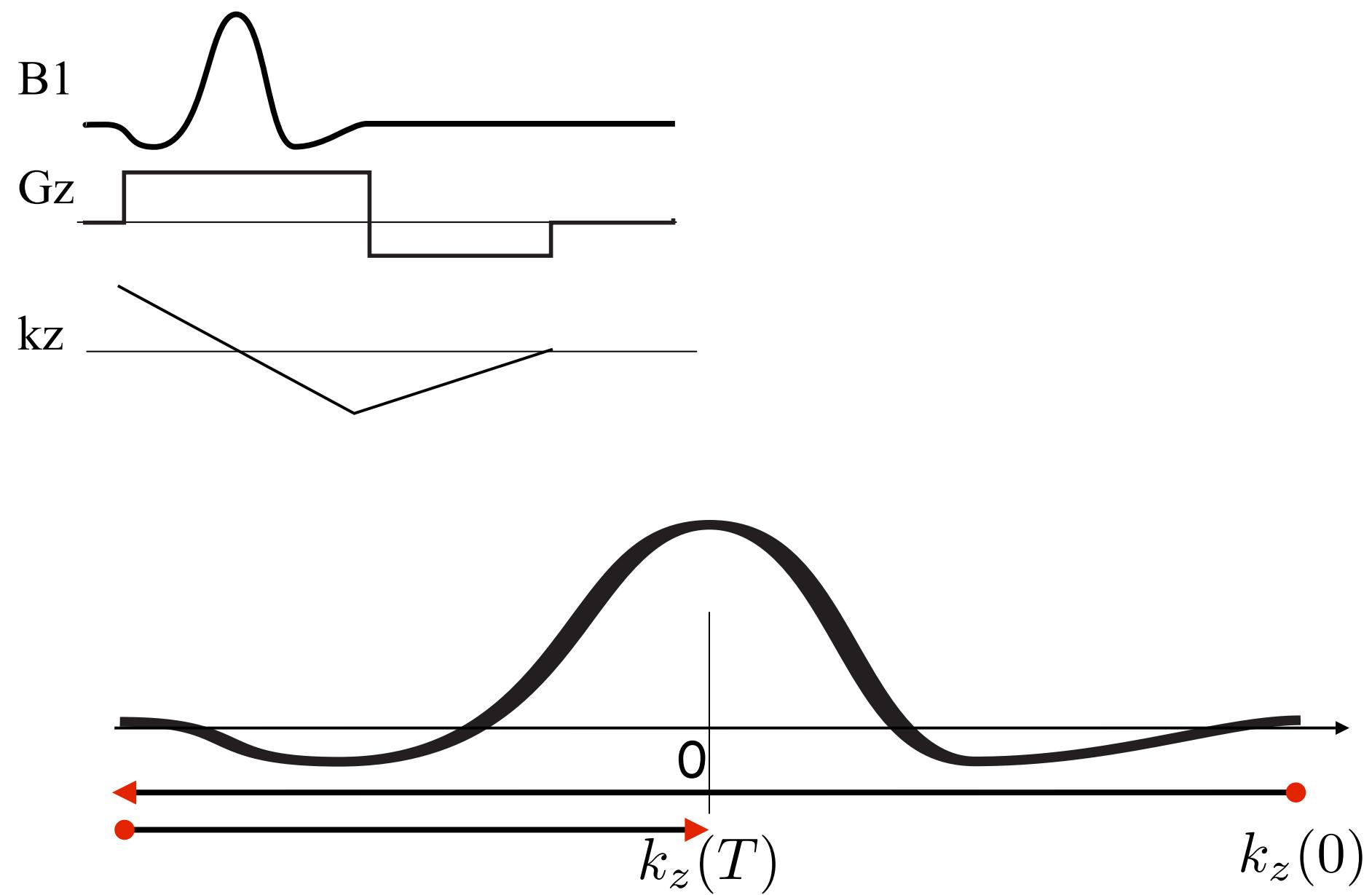
## Example: Slice Selection



- But we get phase across the slice.... signal cancels!

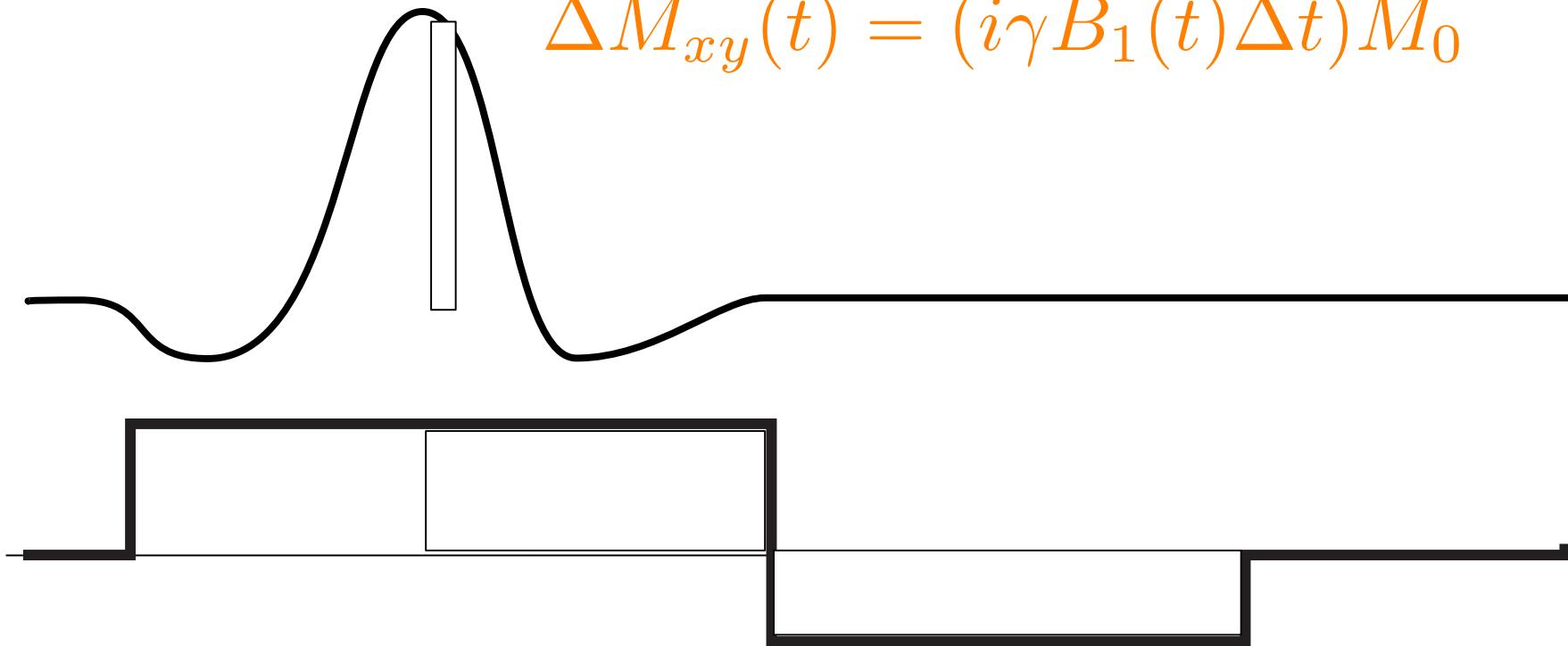


# Slice Refocussing



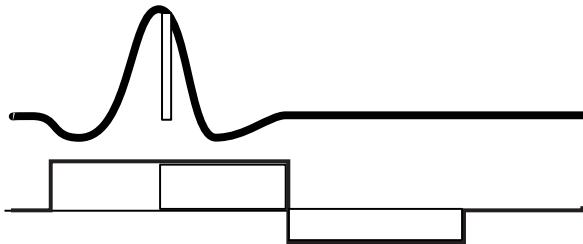
## Graphical Interpretation

$$\Delta M_{xy}(t) = (i\gamma B_1(t)\Delta t)M_0$$



- At each time-point new x-verse magnetization is created
- The new magnetization exhibits precession

## Graphical Interpretation



$$\Delta M_{xy}(t) = (i\gamma B_1(t)\Delta t)M_0$$

$$k_z(t) = \frac{\gamma}{2\pi} \int_t^T G_z(\tau) d\tau$$

area of  
remaining  
gradient

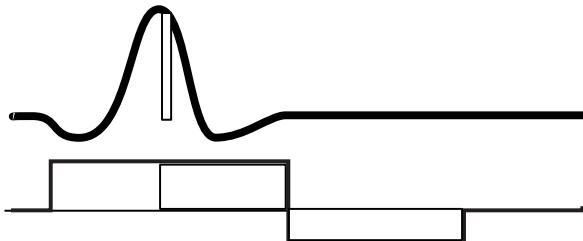
- Magnetization at position z precesses through angle:

$$\theta = -2\pi k_z(t)$$

- Magnetization excited at  $t$ , at position  $z$  will end up:

$$(iM_0\gamma B_1(t)dt)e^{-i2\pi k_z(t)z}$$

## Graphical Interpretation



$$\Delta M_{xy}(t) = (i\gamma B_1(t)\Delta t)M_0$$

- Each magnetization increment is created/precesses independently! Result is the sum of all.
- Sum up magnetizations from  $t=0$  to  $t=T$

$$M_{xy}(z, T) = iM_0 \int_0^T \gamma B_1(t) e^{-i2\pi k_z(t)z} dt$$

## Excitation k-space

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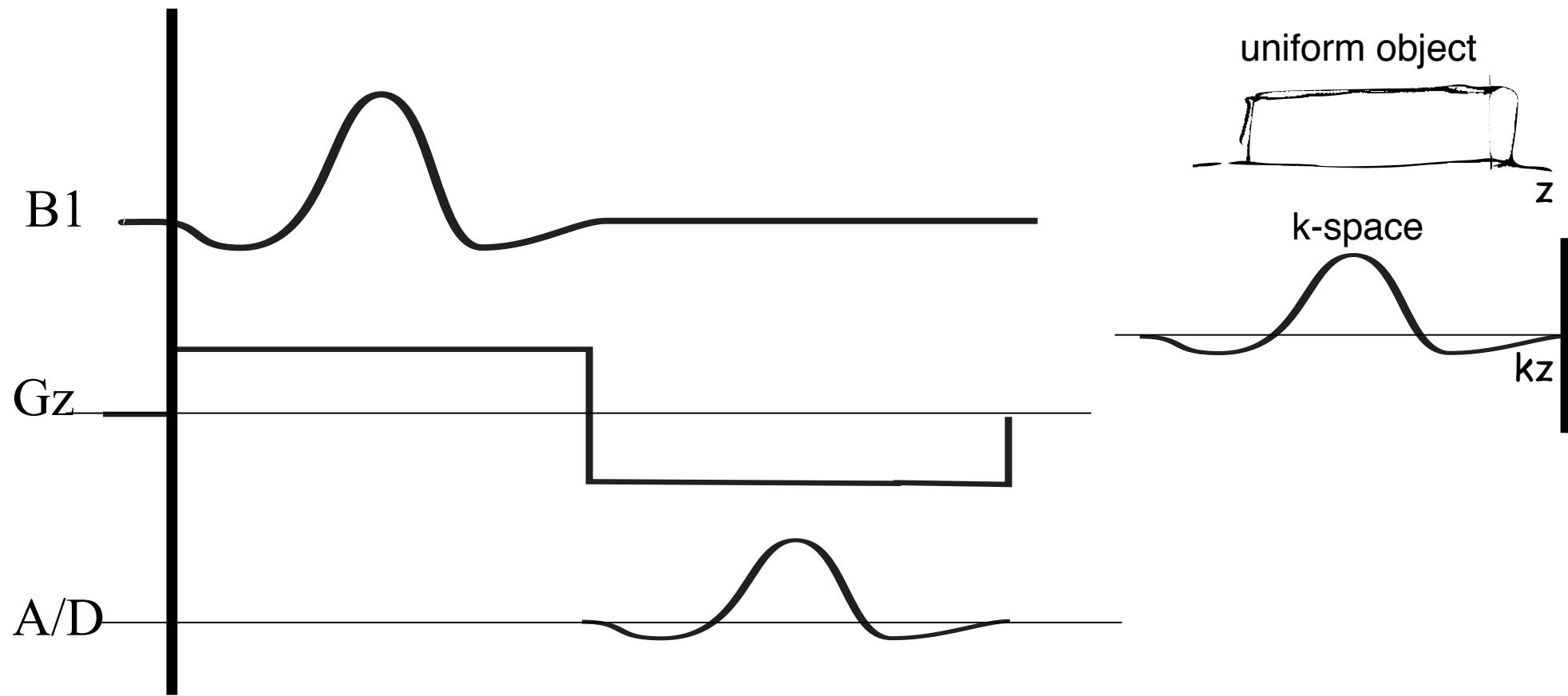
J. Pauly, D. Nishimura and A. Makovski “A k-space analysis of small-tip-angle excitation” JMR, 1989;81:43-56



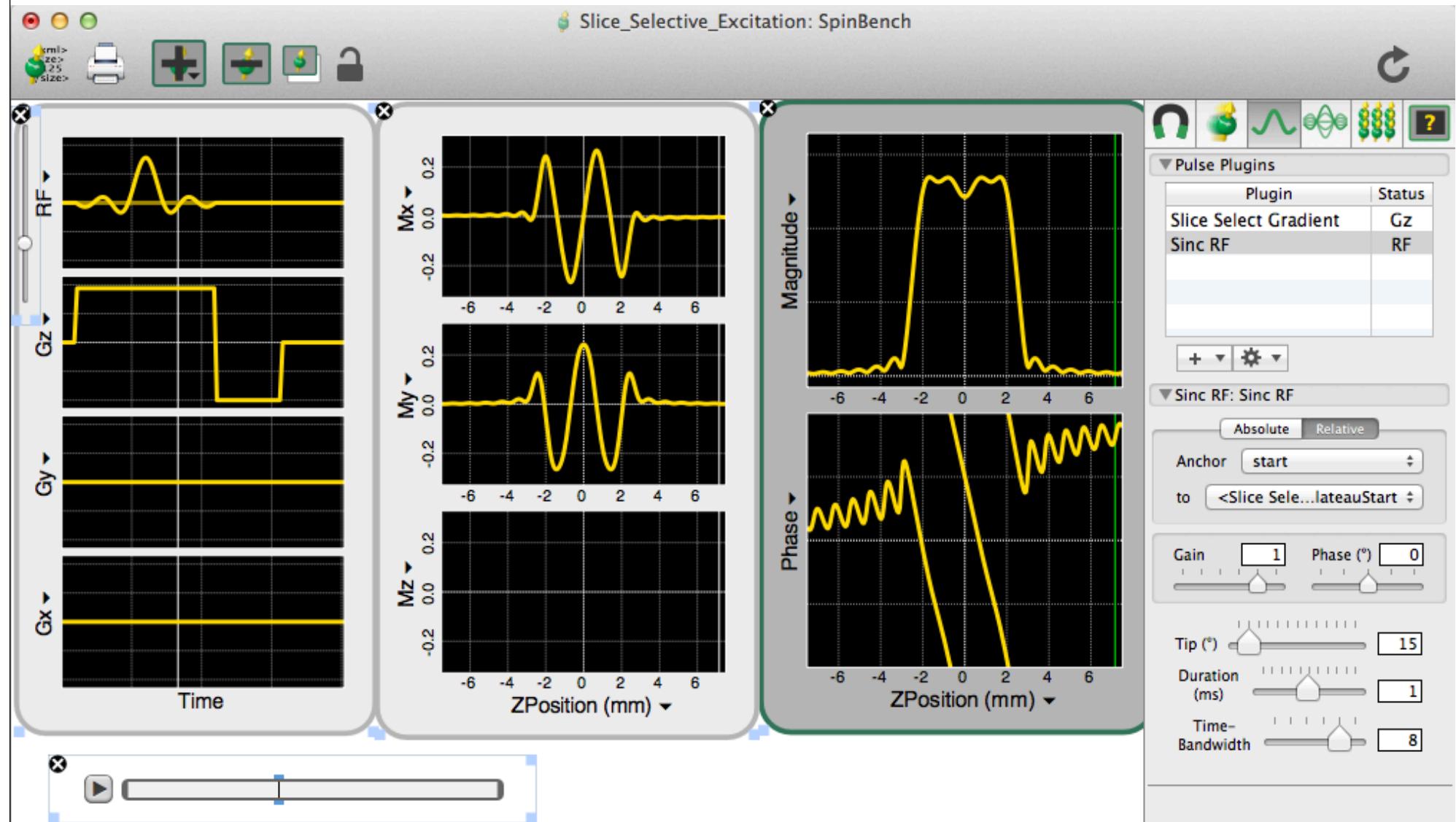
\* Slightly different conventions than we used.

## RF and readout

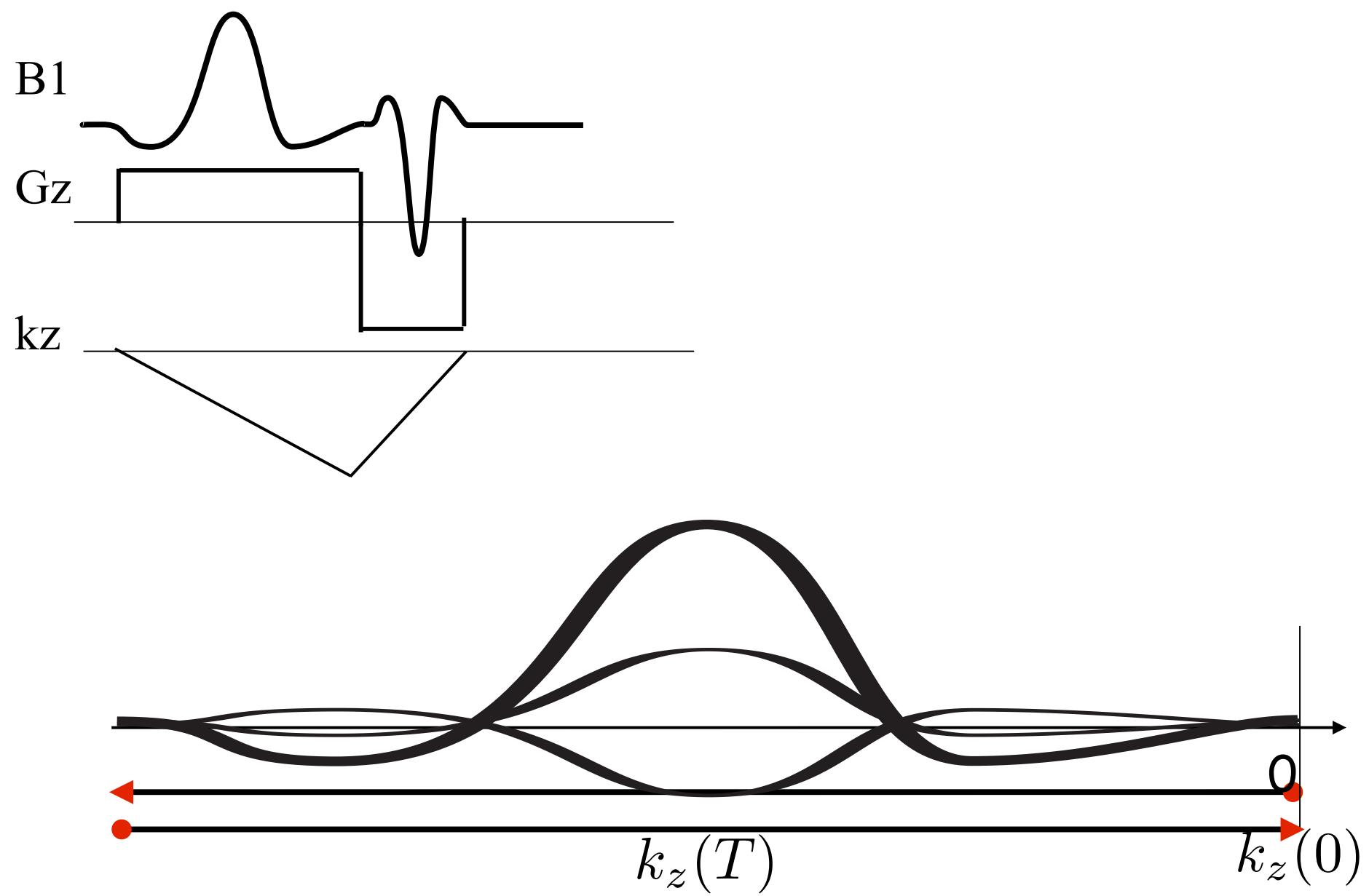
- RF burns magnetization in k-space
- Receive reads the burned magnetization (weighted by object)



# Spin Bench simulation



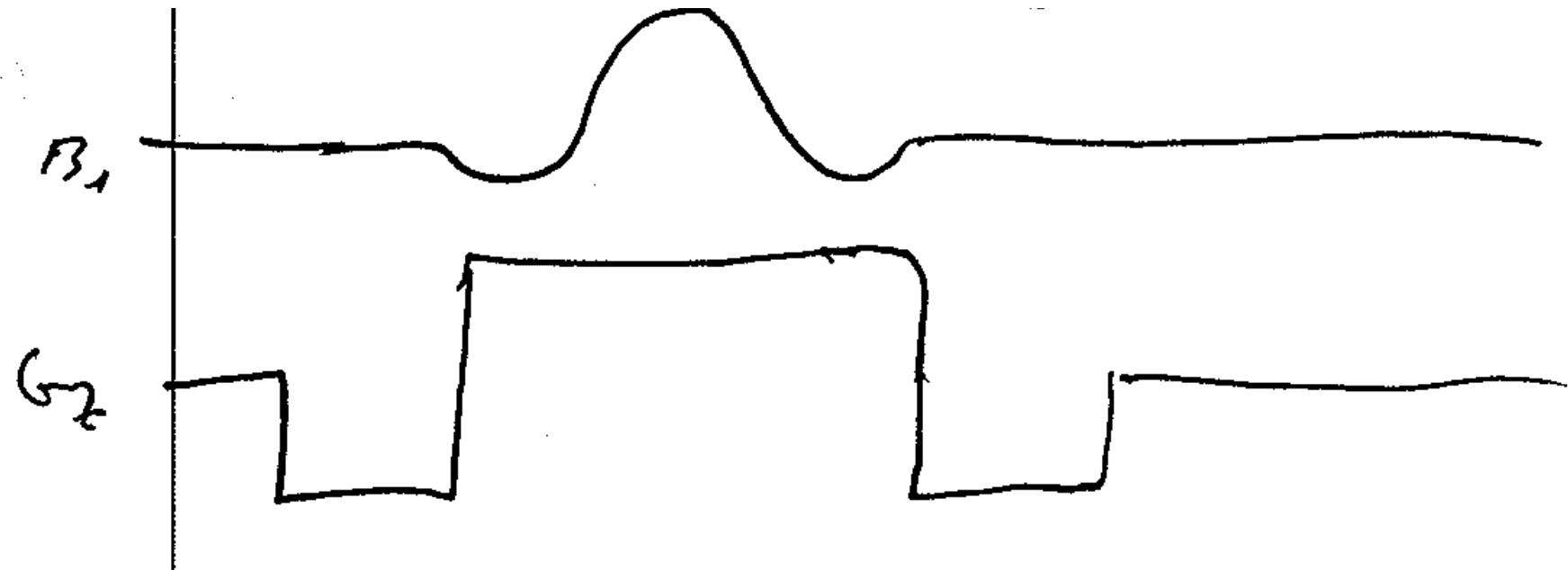
# k-Space Weighting Example



## Examples

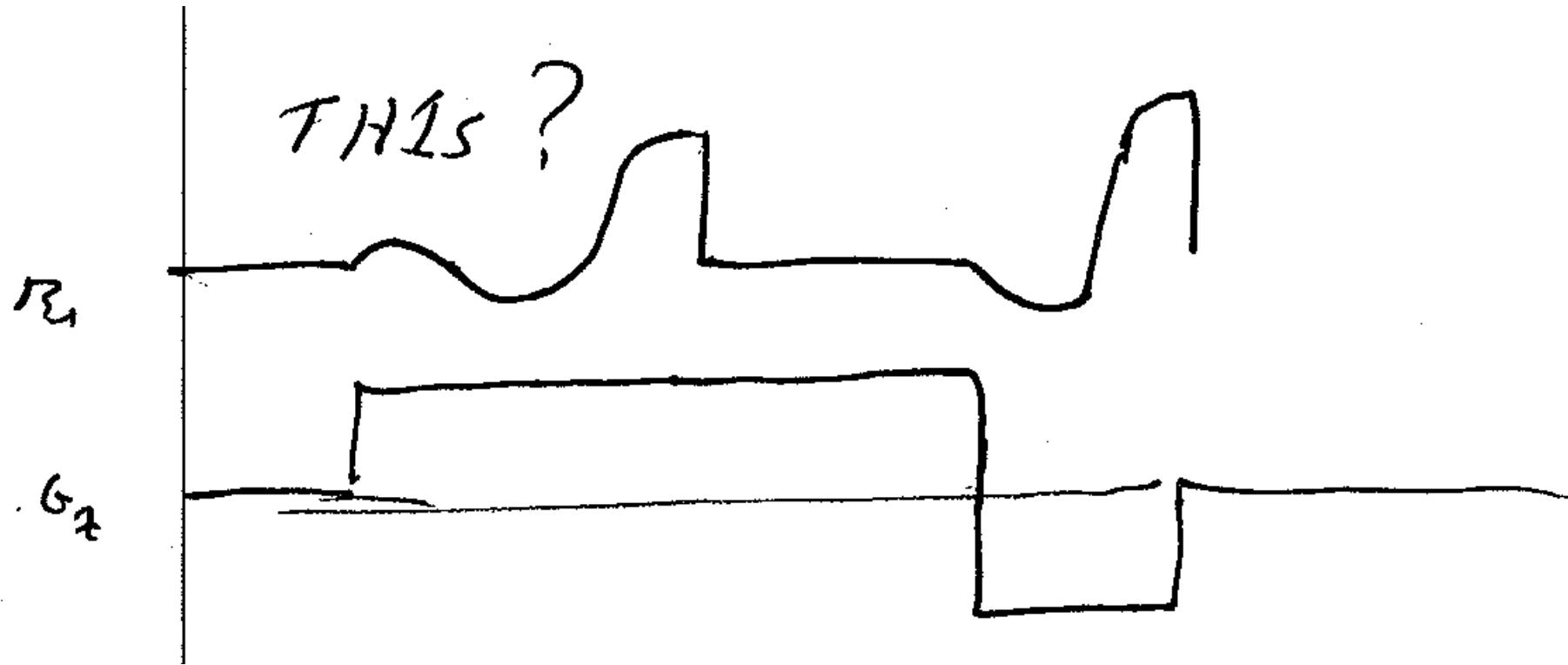
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What does this do?



## Examples

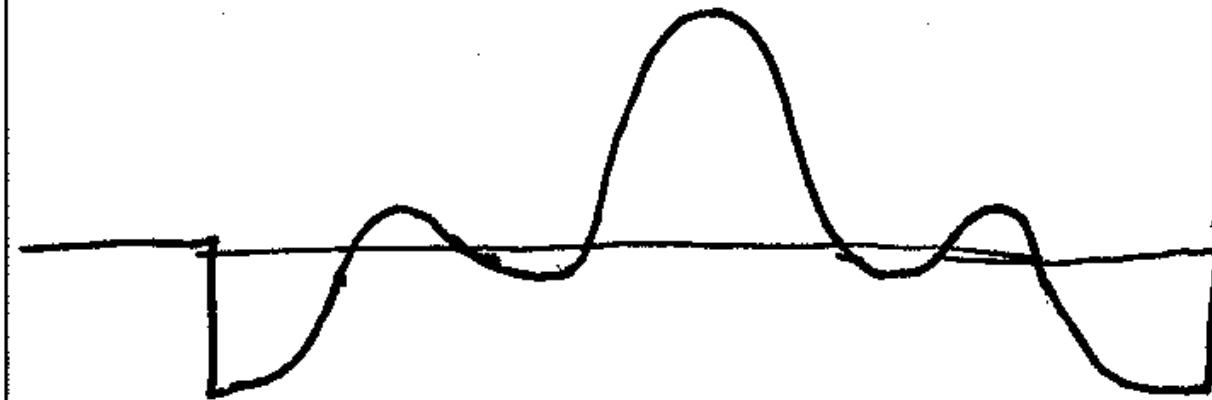
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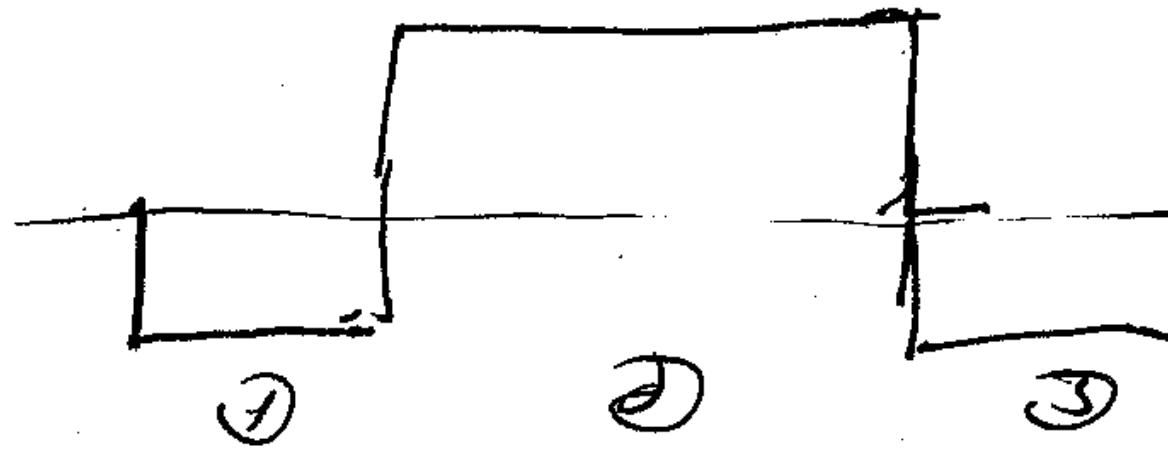
Exan

THIS!

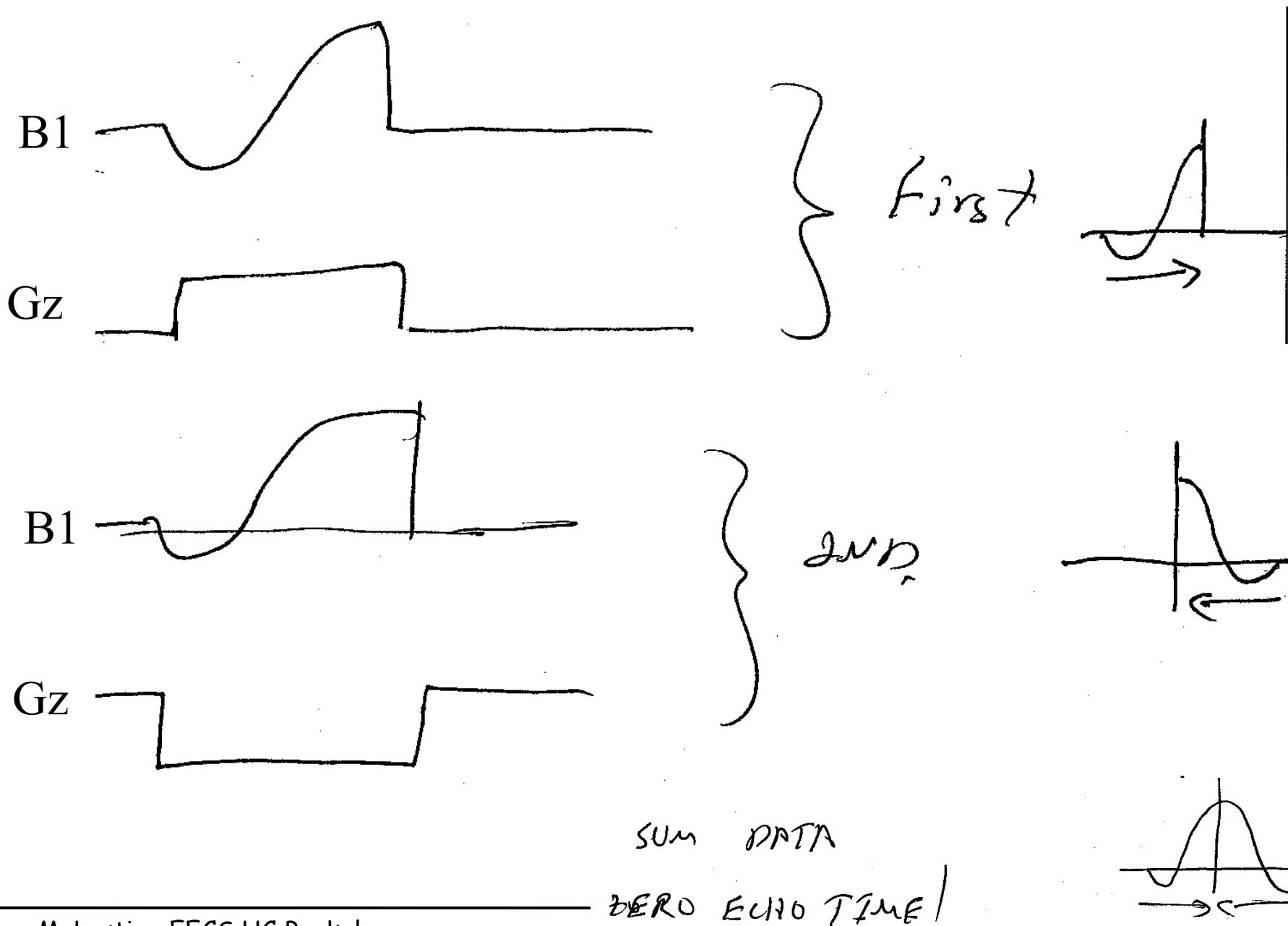
B<sub>1</sub>



G<sub>7</sub>

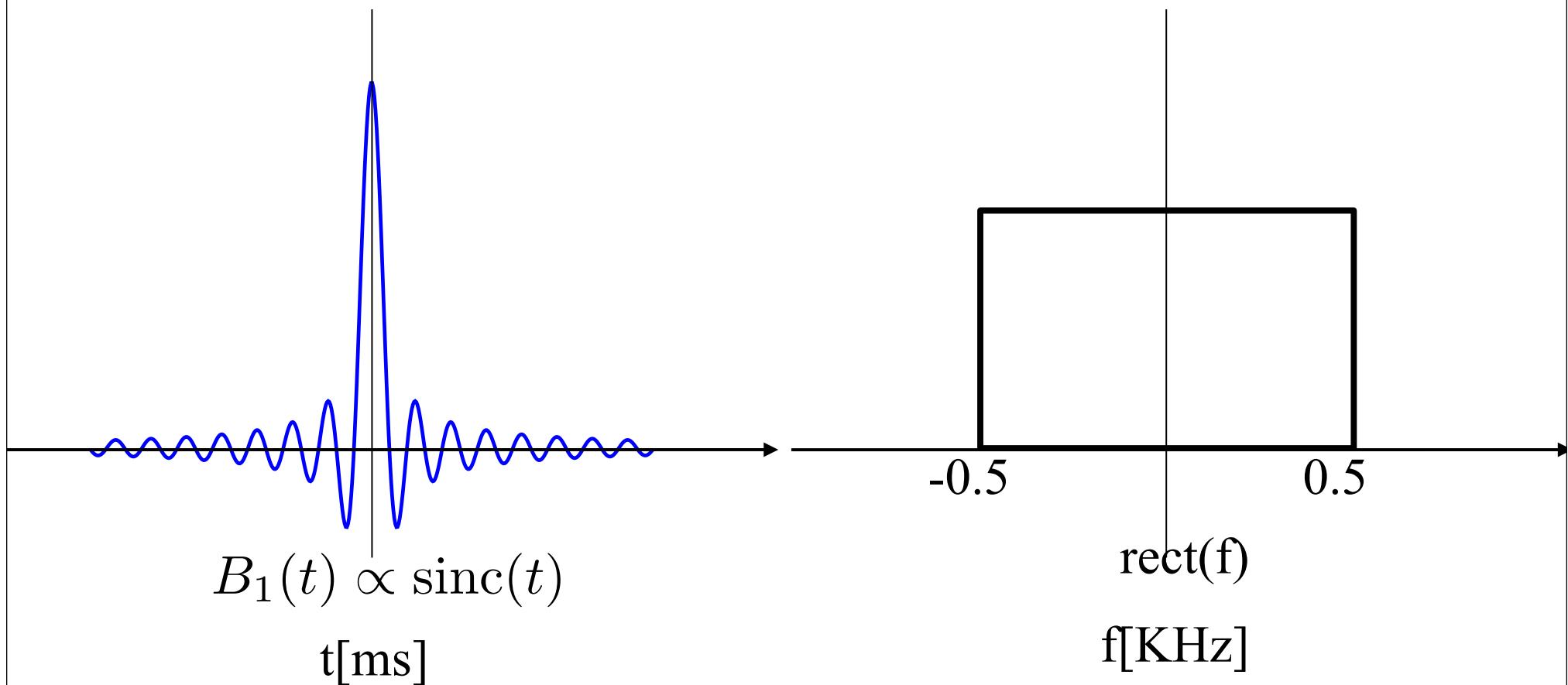


# Multiple Excitations



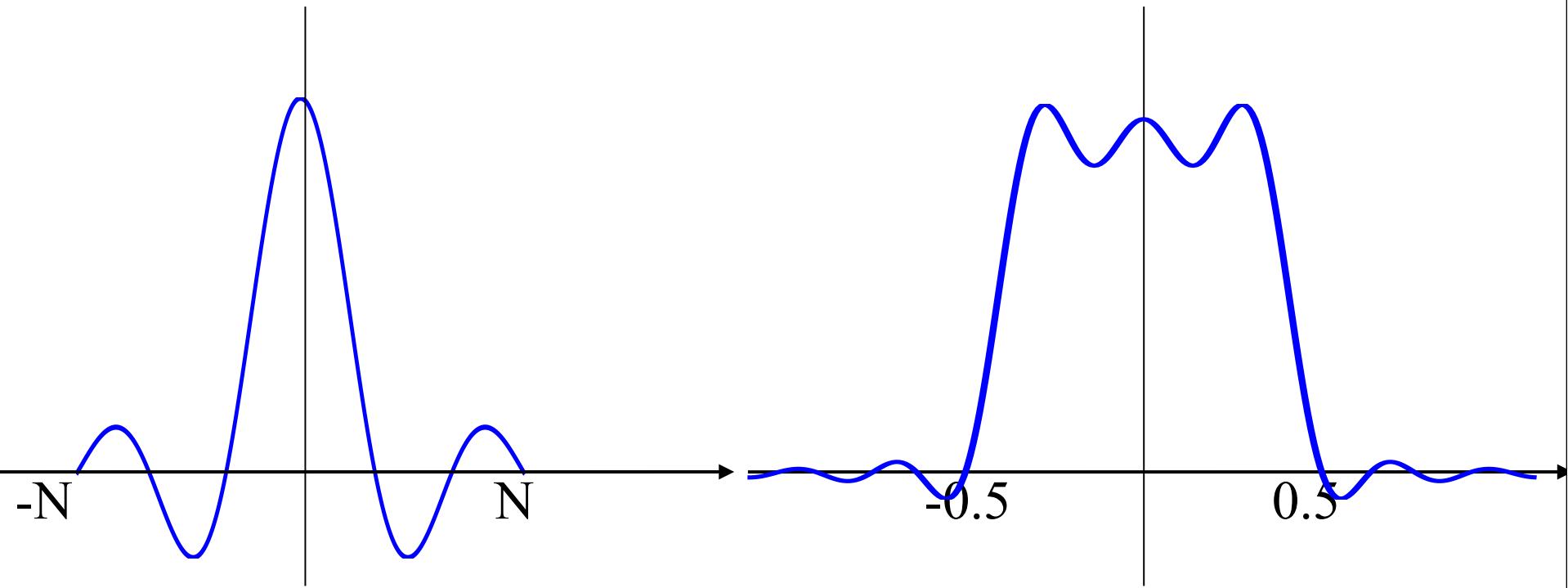
## RF Pulse Design

- Choose,  $B_1(t)$  with a nice transform



Not practical, since sinc is continuous indefinitely

## Truncated sinc

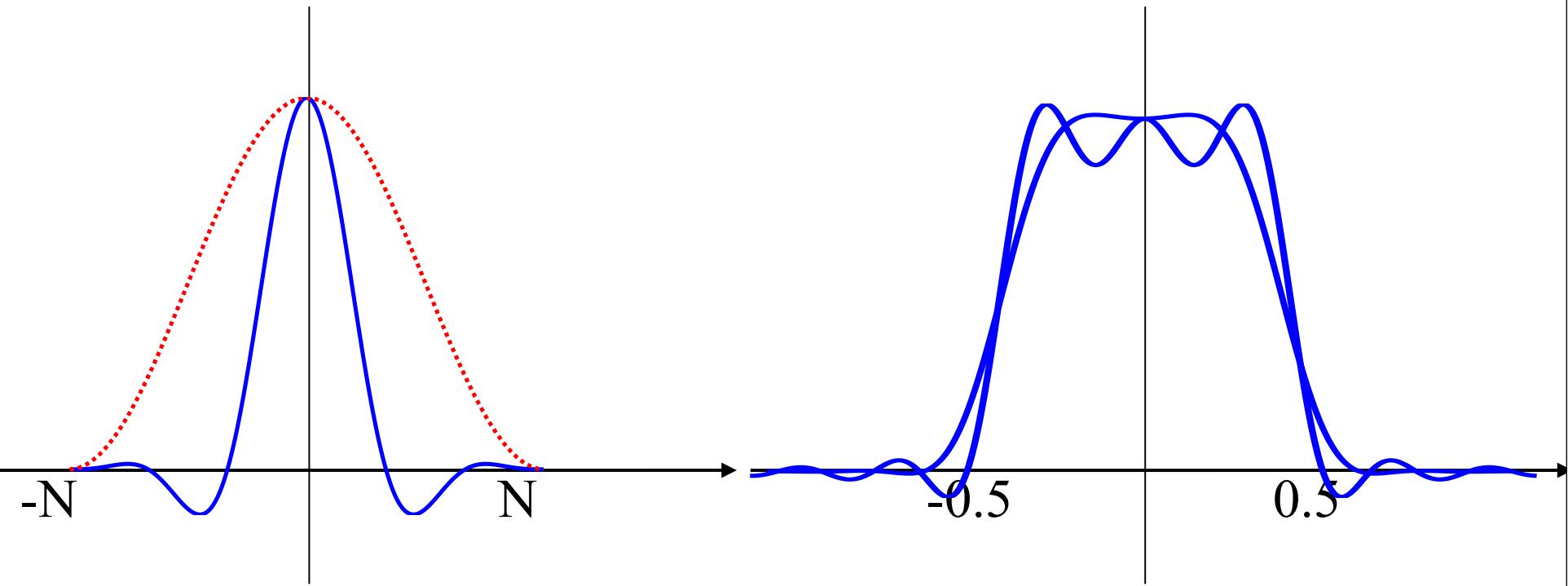


$$B_1(t) \propto \text{sinc}(t)\text{rect}(t/2N)$$

$$\text{rect}(f)^* 2N \text{sinc}(2Nf)$$

Too much Ripple!

# Windowed sinc



$$B_1(t) \propto \text{sinc}(t)w(t/2N)$$

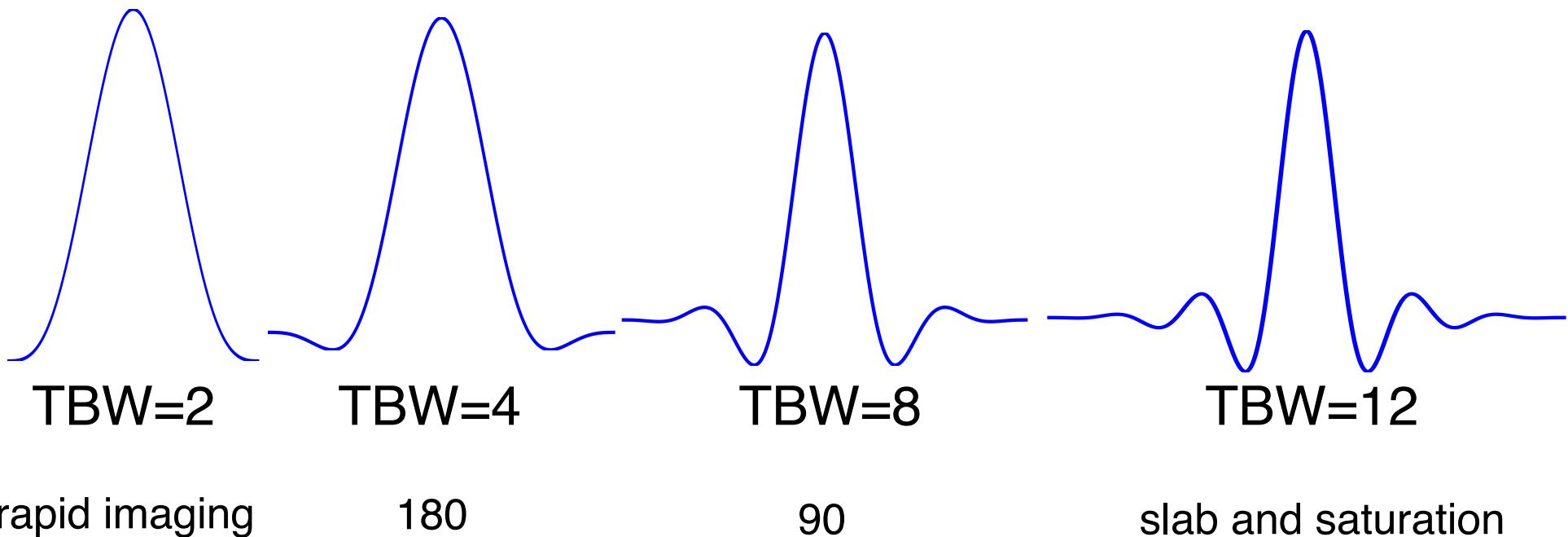
$$\text{rect}(f)^*2N W(2Nf)$$

Hanning Window

# Characterization of Pulse Shape

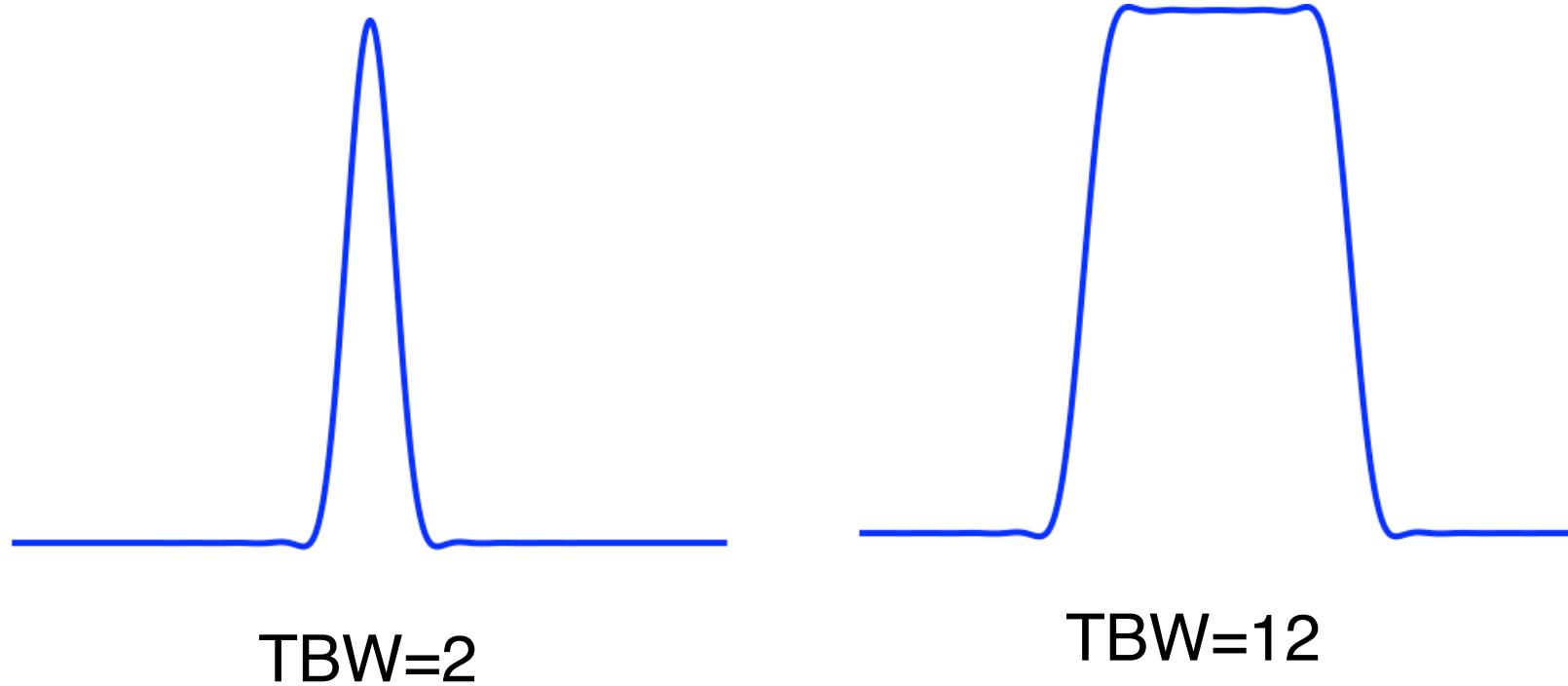
Time-Bandwidth Product

$$T(BW) = (2N)1 = 2N \Rightarrow \text{Total # of zero crossings}$$

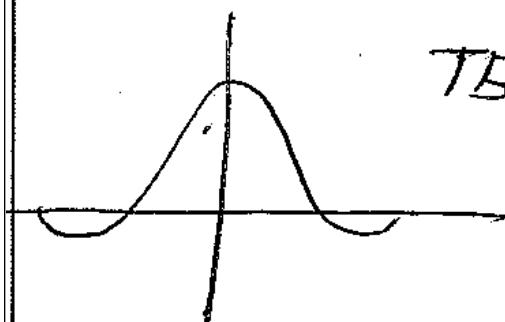


# Slice Profile

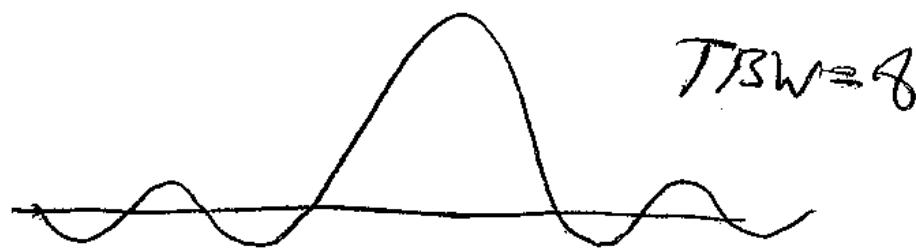
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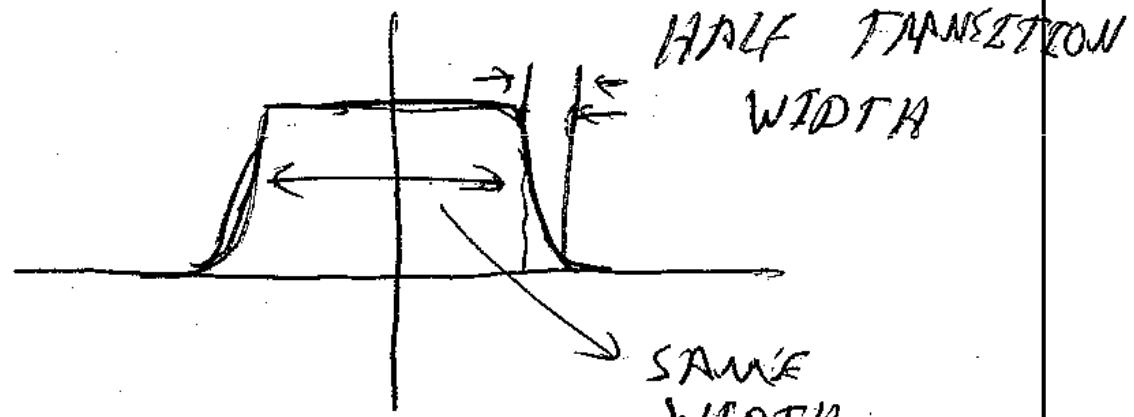
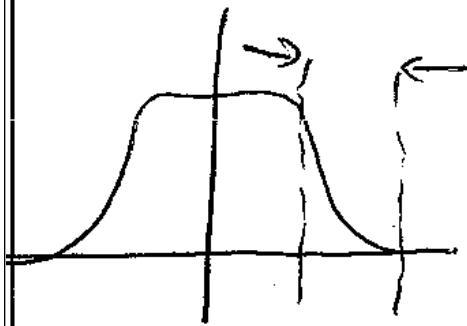
IF WE FIX BANDWIDTH AND MAKE T LONGER



TBW=4

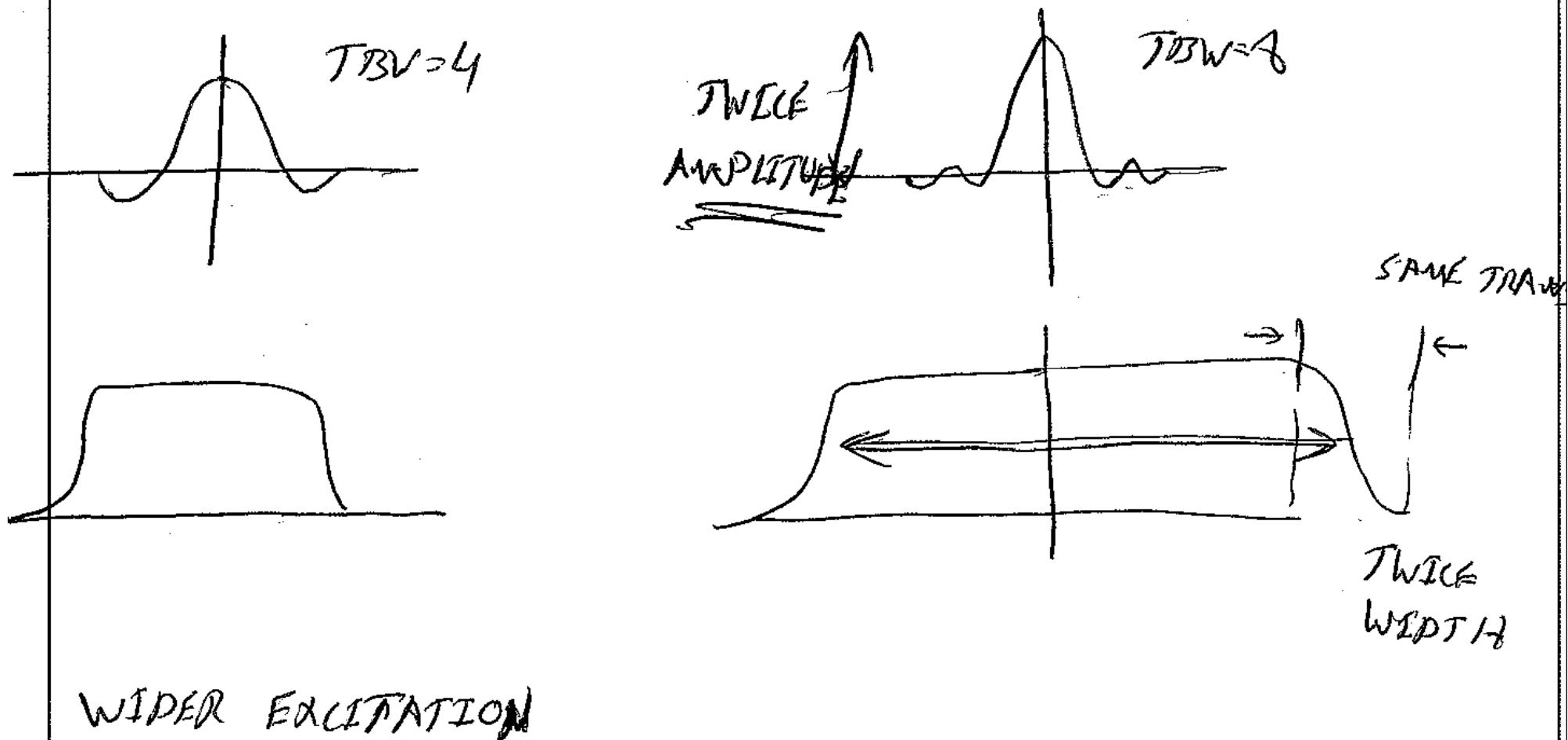


TBW=8



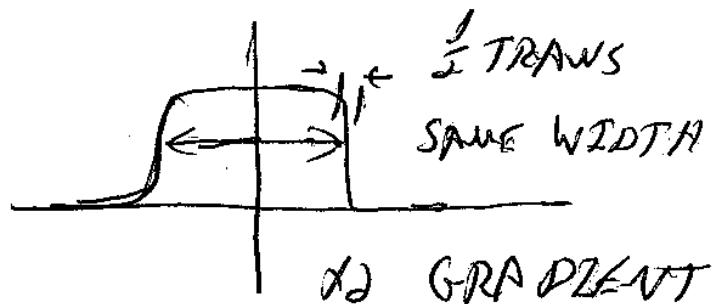
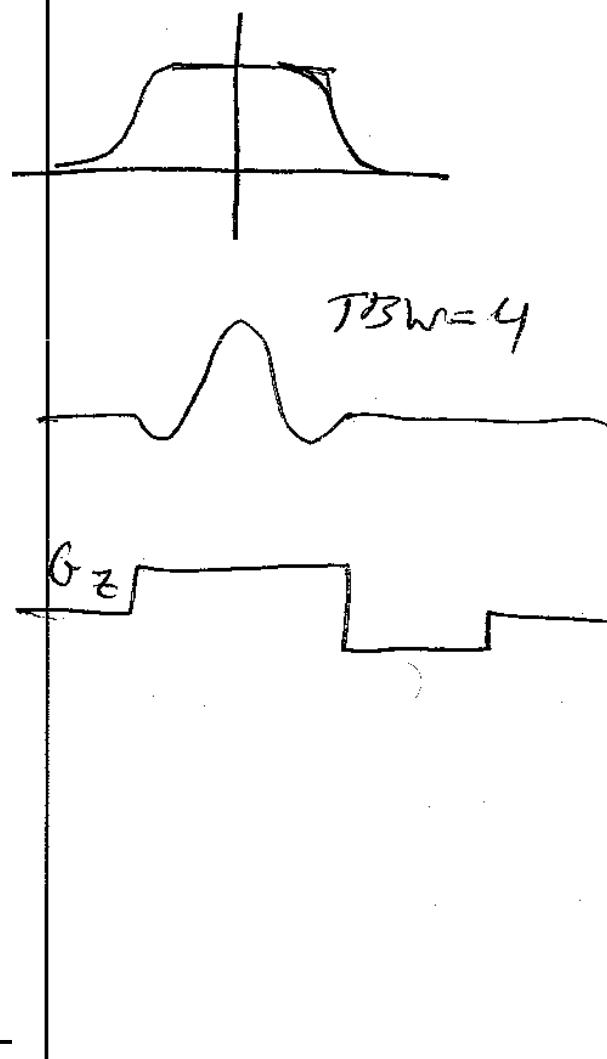
MORE SELECTIVE PROFILE.

IF WE FIX DURATION INCREASE BW



WIDER EXCITATION

TYPICALLY IN MRI WE FIX DURATION, AND  
ADJUST THE GRADIENT AMP. TO COMPENSATE FOR  
FOR THE INCREASE IN BW



$\Delta G_z$

DOUBLE BW (kHz)  
DOUBLE GRADIENT (kHz/ch)  
⇒ SAME WIDTH !

## EXAMPLE

WE WANT A  $T_{BW} = 8$  PULSE WITH  $4\text{ms}$  DURATION

SLICE THICKNESS IS  $1\text{cm}$ , WHAT IS THE GRADIENT AMPL?

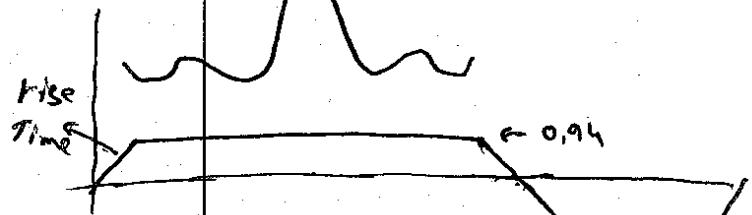
$$T(BW) = 8$$

$$\Delta_{ms} \text{ BW} = 8 \Rightarrow BW = 4\text{kHz}$$

$$\Delta z = 1\text{cm}$$

$$\underbrace{\frac{\partial}{\partial t} G \Delta z}_{BW} = 4\text{kHz}$$

$$(4.257 \frac{\text{kHz}}{\text{s}}) G \cdot (1\text{cm}) = 4\text{kHz} \Rightarrow G = 0.94 \frac{\text{G}}{\text{cm}}$$



Q. WHAT IS  $G$  IF SLICE =  $0.5\text{cm}$ ?

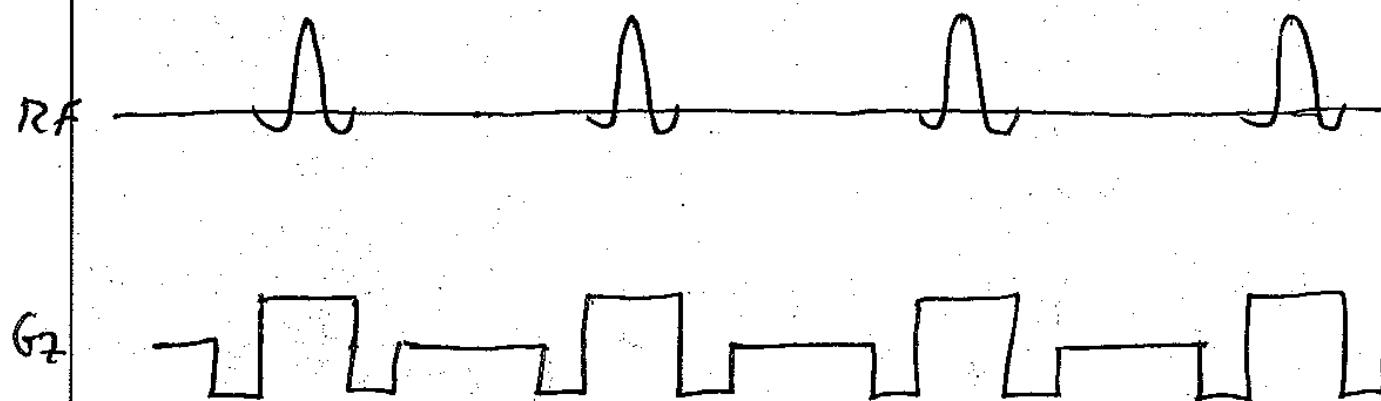
A.  $G = 1.48 \frac{\text{G}}{\text{cm}}$

Q. WHAT IF  $G_{max} = 0.94 \frac{\text{G}}{\text{cm}}$ ?

$T_{BW} = 4 \Rightarrow$  LESS SELECTIVE

$T = 4\text{ms} \Rightarrow$  LONGER DURATION.

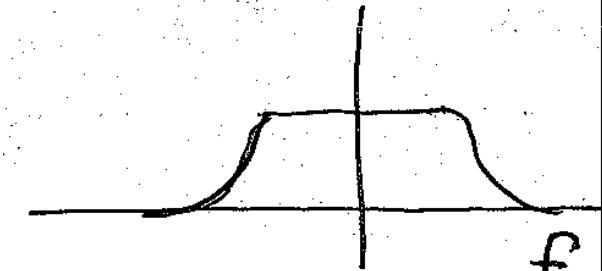
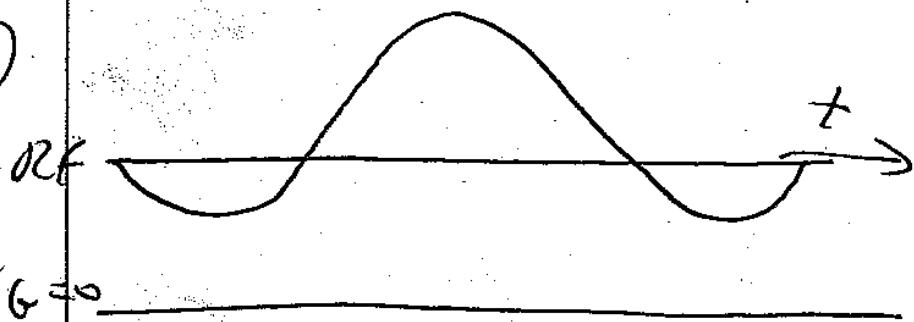
WHAT DOES THIS PULSE DO?



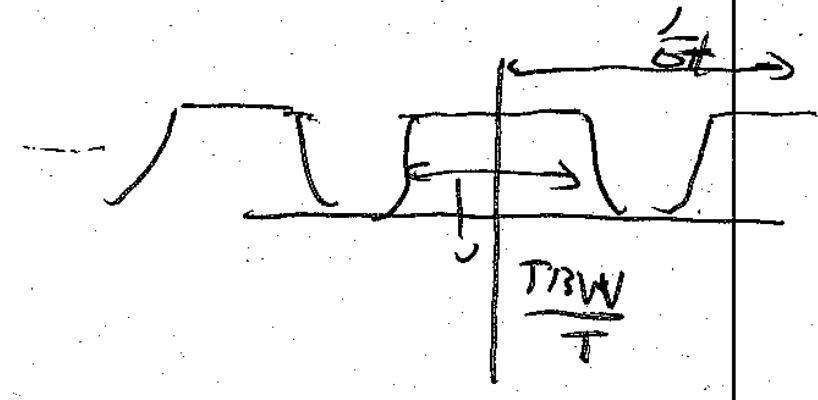
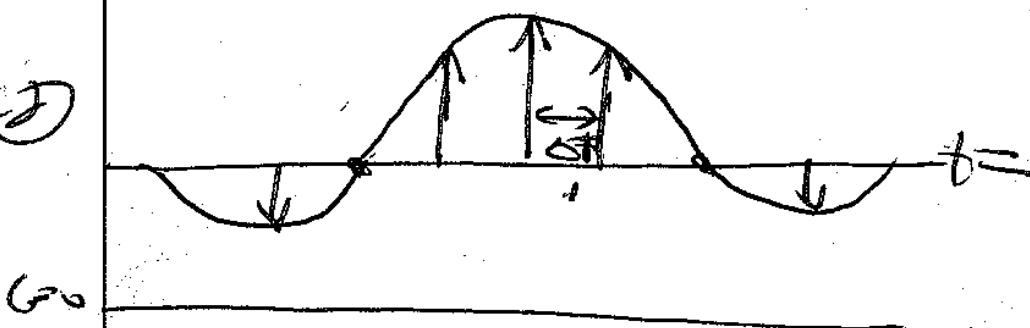
## SPECTRAL PULSE

WHAT DO THESE PULSES DO?

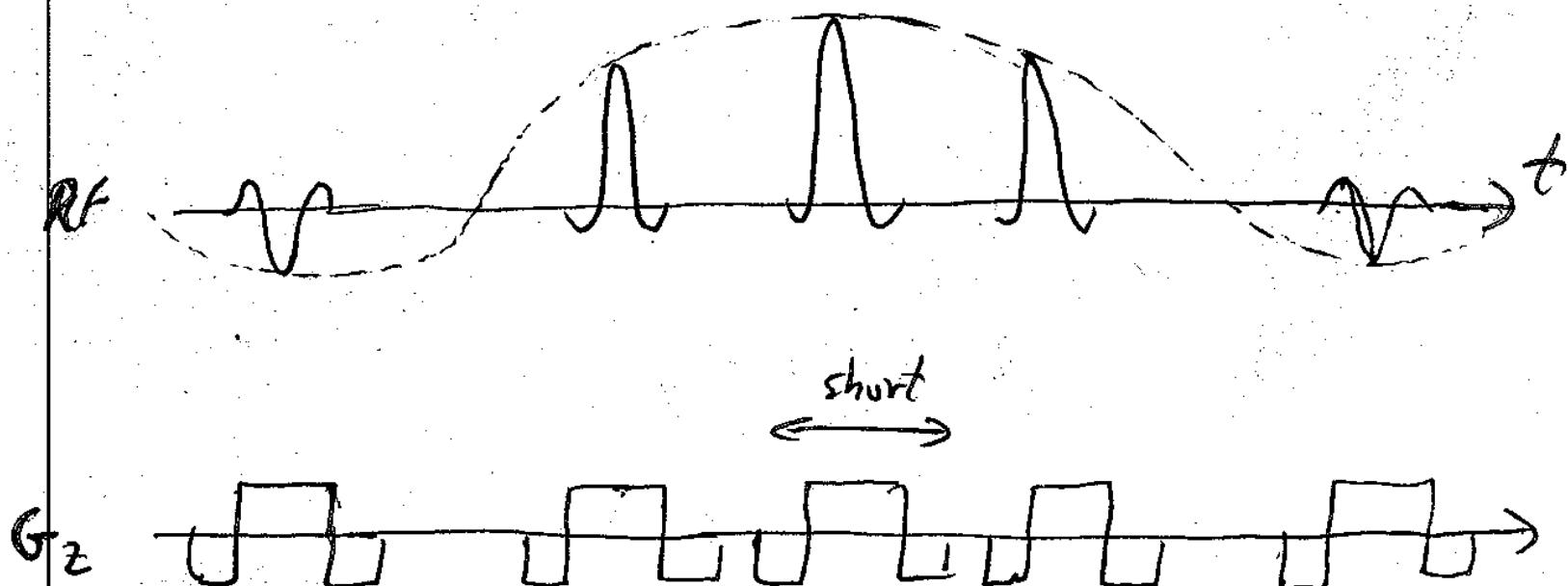
①



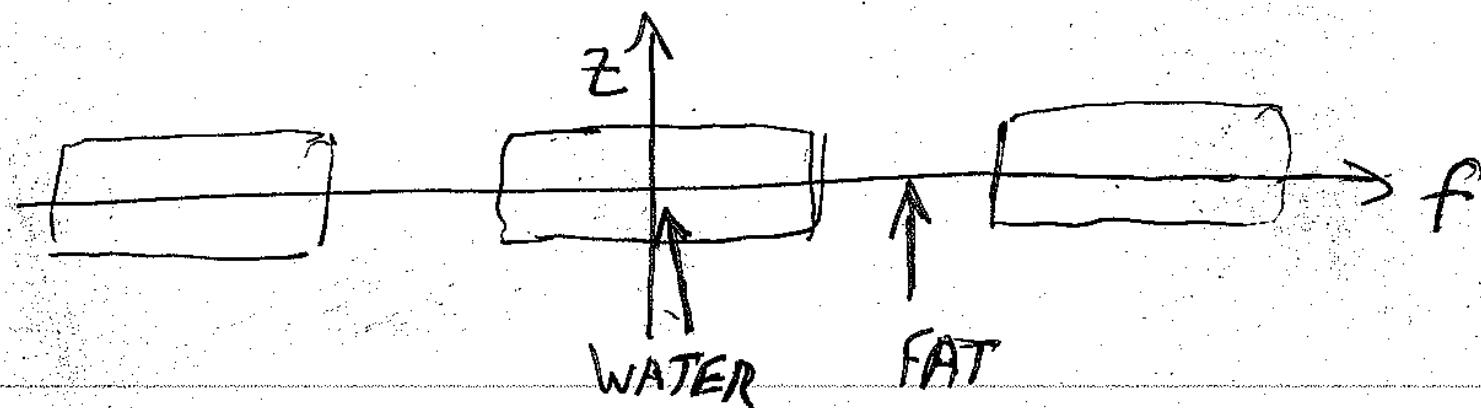
②



REPLACE HARD RF WITH SLICE SELECT SUB-PULSES



SPATIAL AND SPECTRAL SELECTIVITY!



WHAT HAPPENS AT LARGE FLAPS?

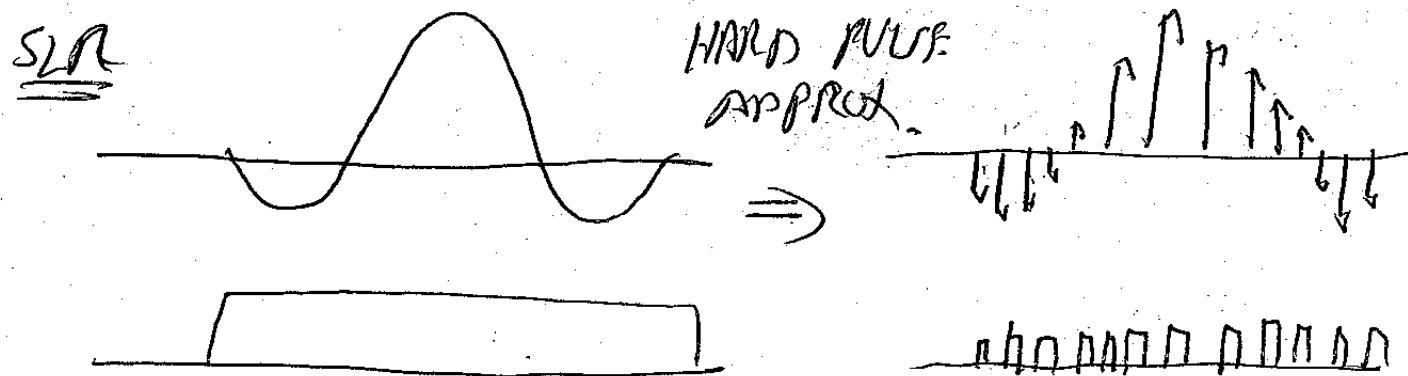
MANY METHODS:

- NUMERICAL OPTIMIZATION
- OPTIMAL CONTROL (CONVEX)
- SLR (PAULY)
- PERTURBATION THEORY

OPTIMAL CONTROL:

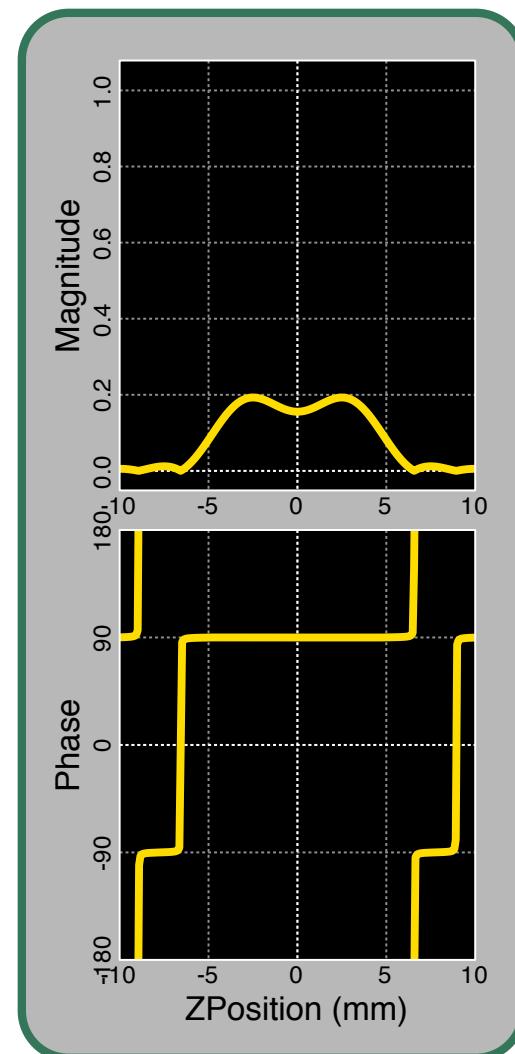
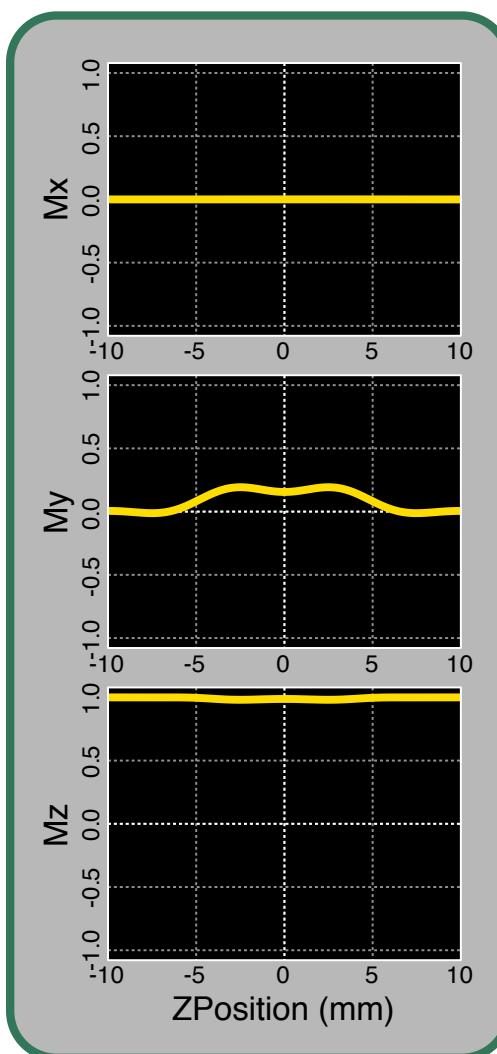
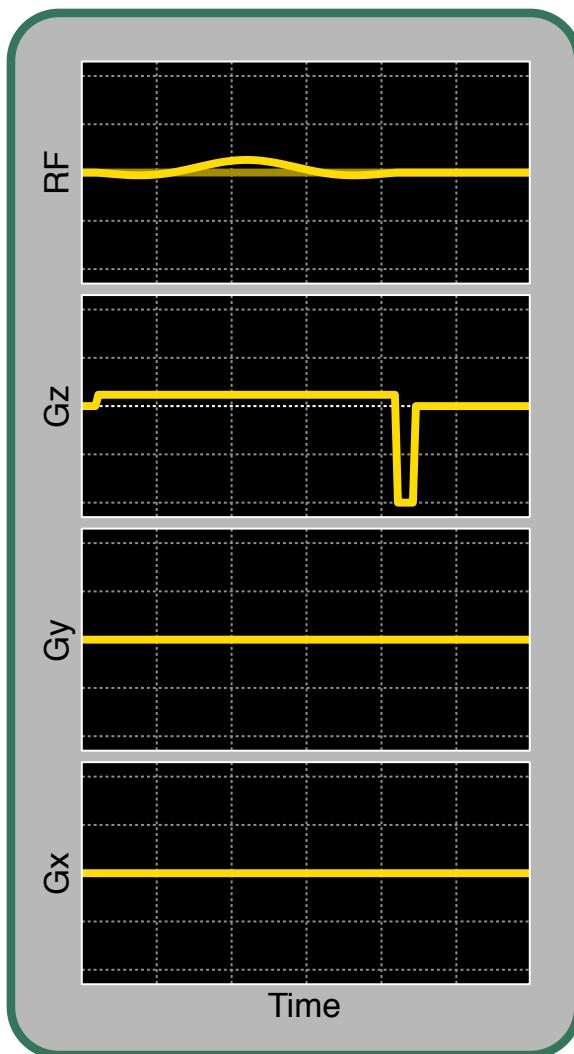
$$\begin{pmatrix} \dot{x}_1 \\ \dot{x}_2 \\ \dot{x}_3 \end{pmatrix} = \begin{pmatrix} 0 & \vec{f}(\vec{r}) & -\delta B_{11}y \\ -\delta B_{11}^T & 0 & \delta B_{12} \\ \delta B_{12} & 0 & 0 \end{pmatrix} \begin{pmatrix} x_1 \\ x_2 \\ x_3 \end{pmatrix}$$

Design  $\vec{f}(b)$ ,  $\delta(b)$  to move spms  
at positions  $\vec{r}$  to desired position

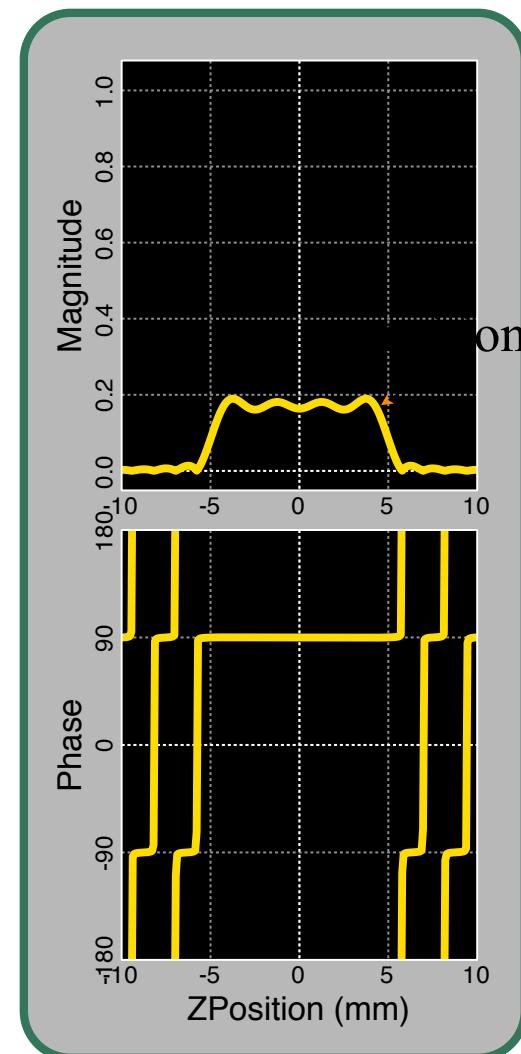
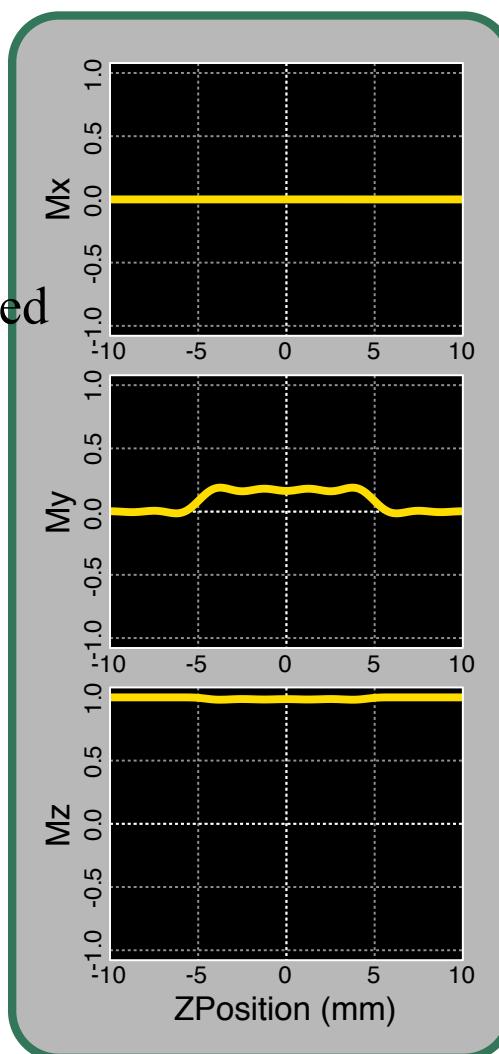
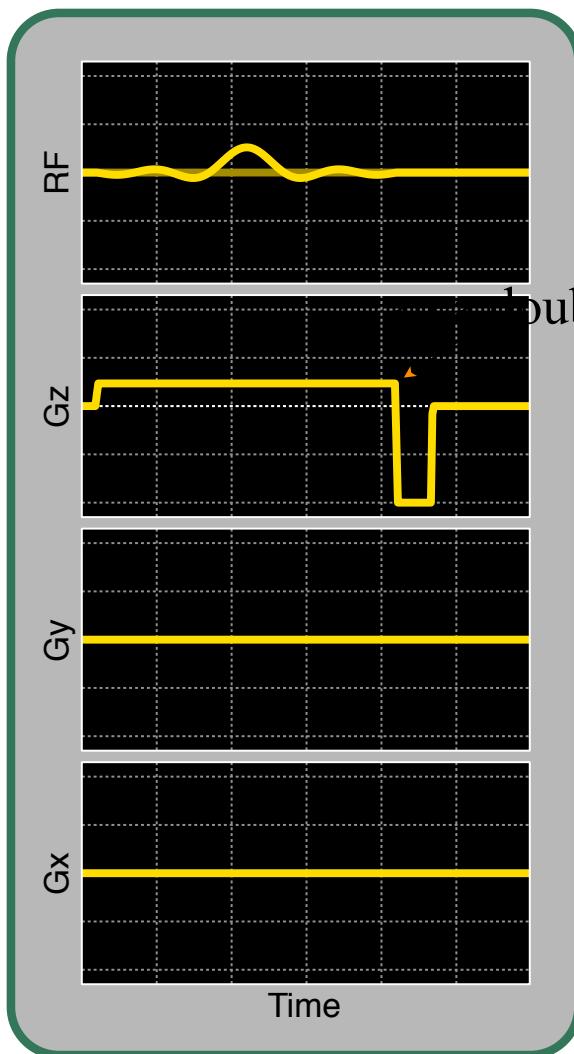


GOOD THINGS HAPPEN!

$TBW=4$ , flip = 10, slice = 10mm, duration =2ms

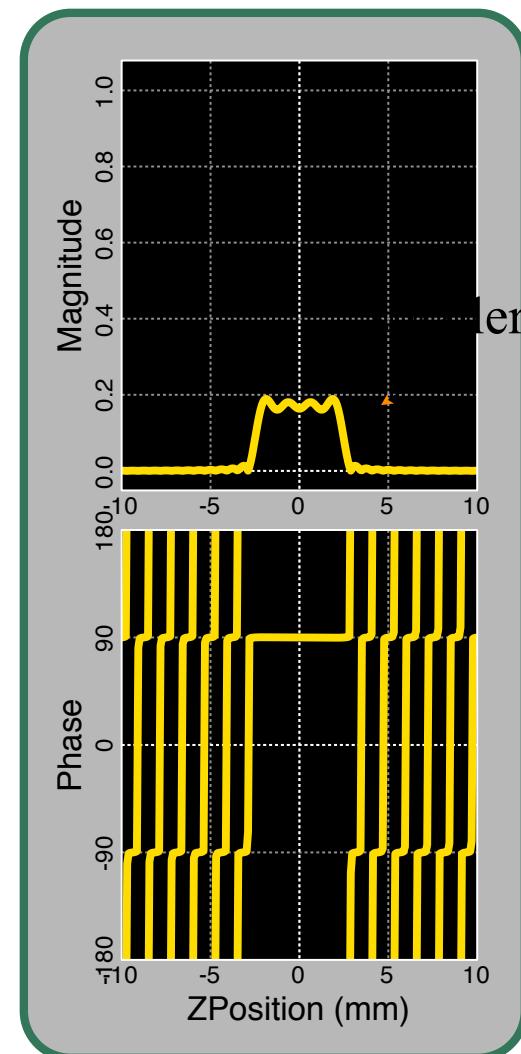
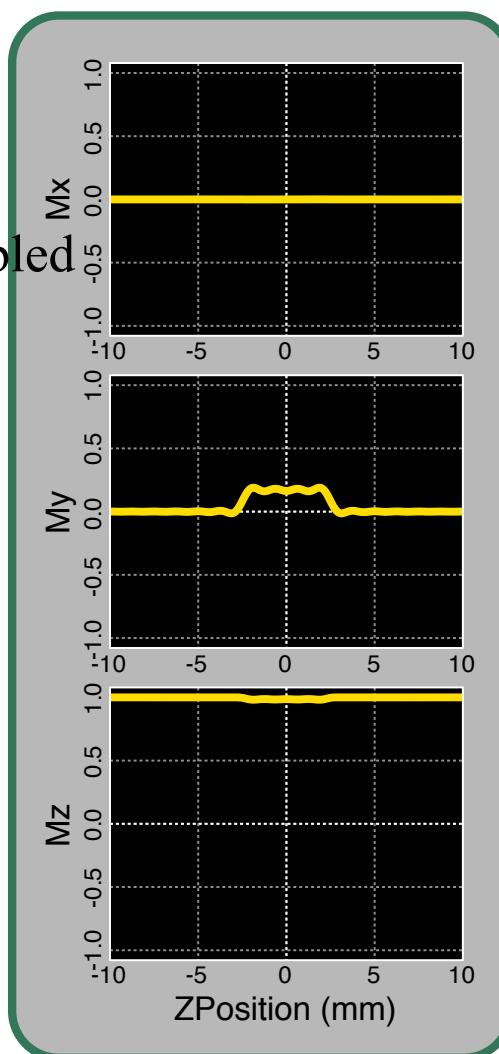
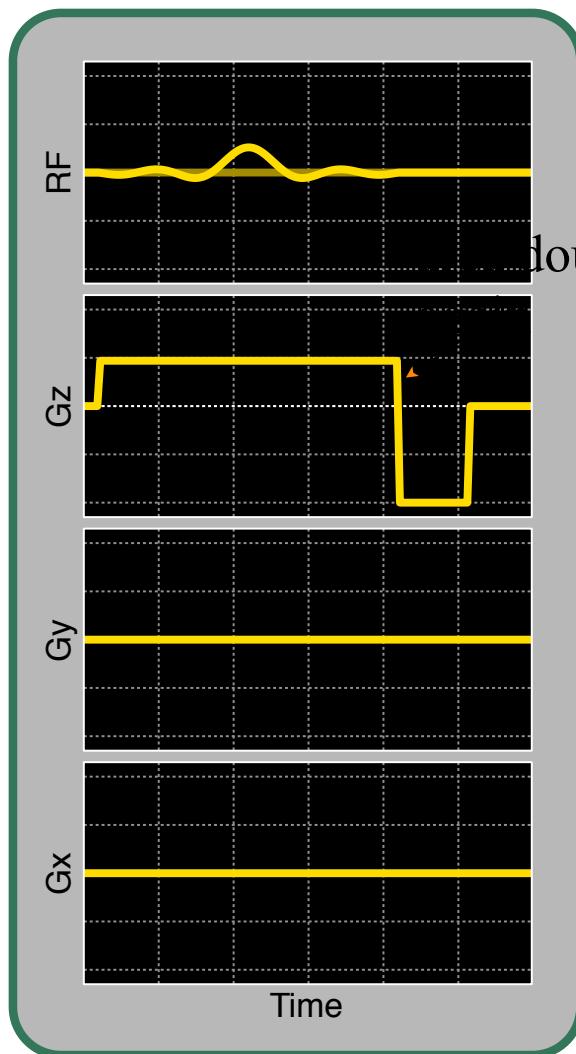


$\text{TBW}=8$ , flip = 10, slice = 10mm, duration =2ms



on halved

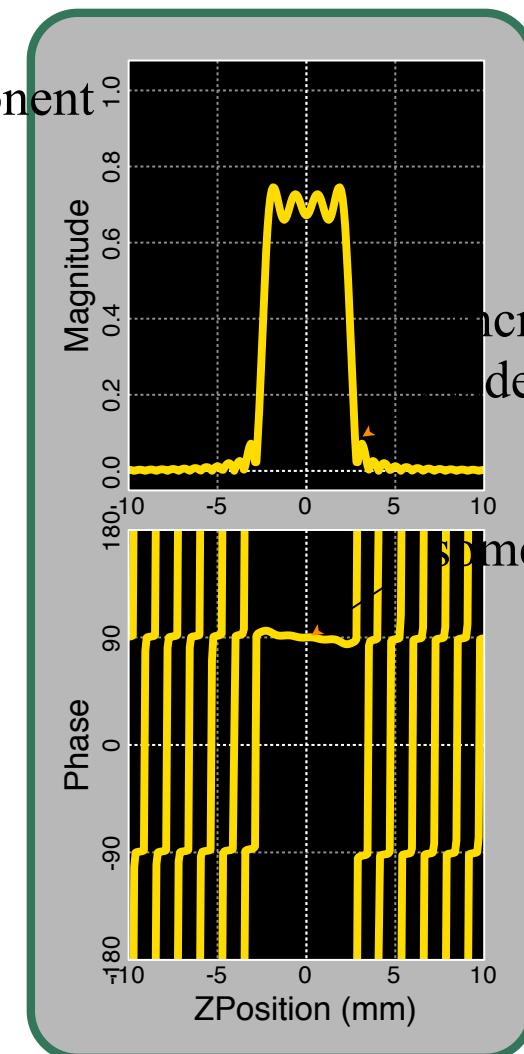
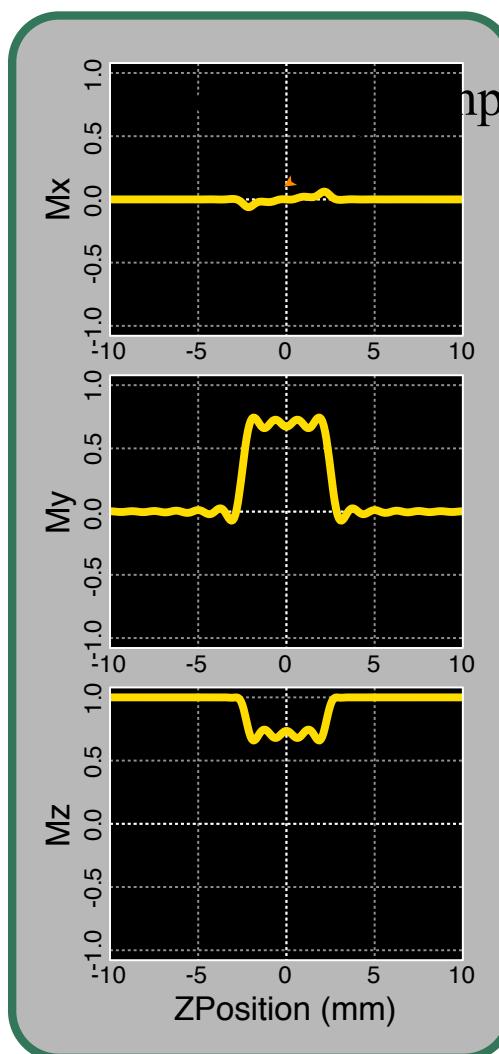
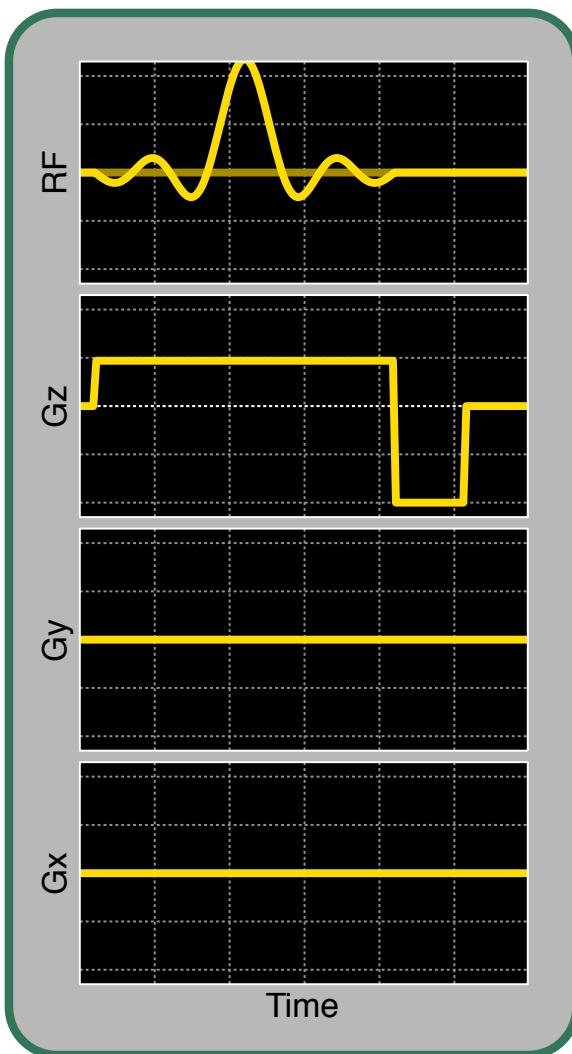
$\text{TBW}=8$ , flip = 10, slice = 5mm, duration =2ms



doubled

per slice

TBW=8, flip = 45, slice = 5mm, duration =2ms

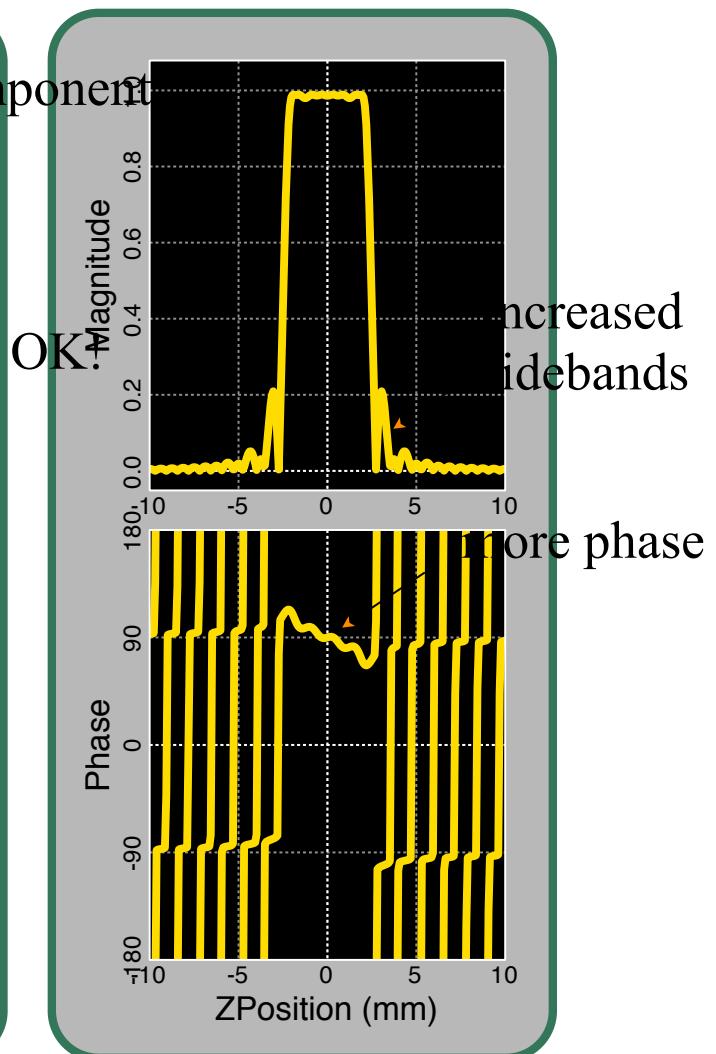
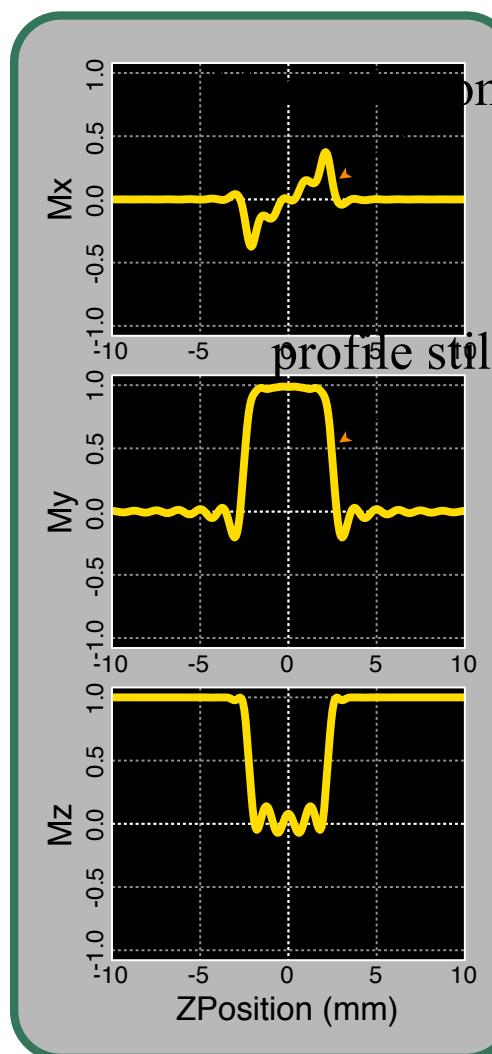
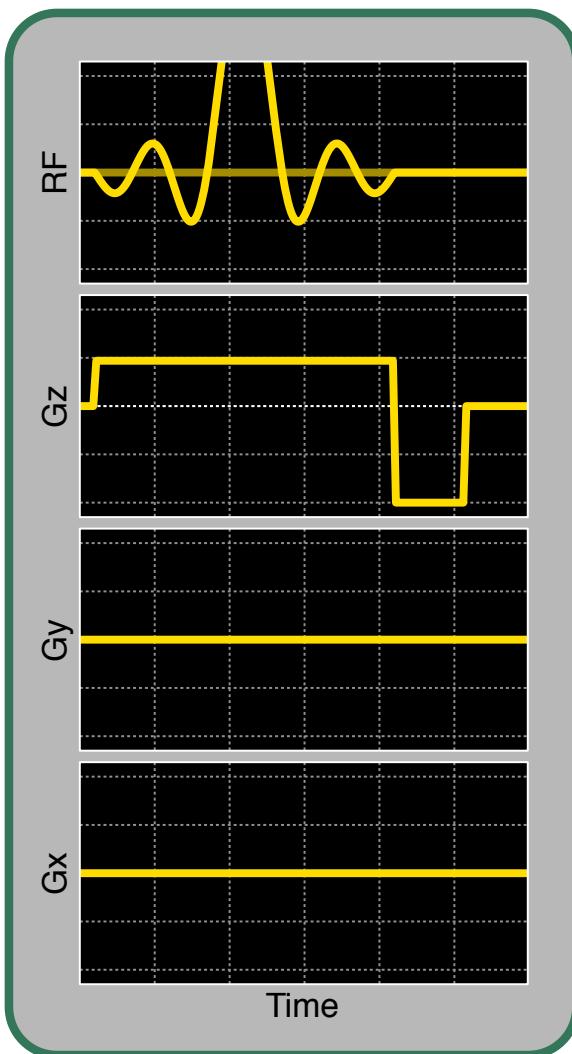


component

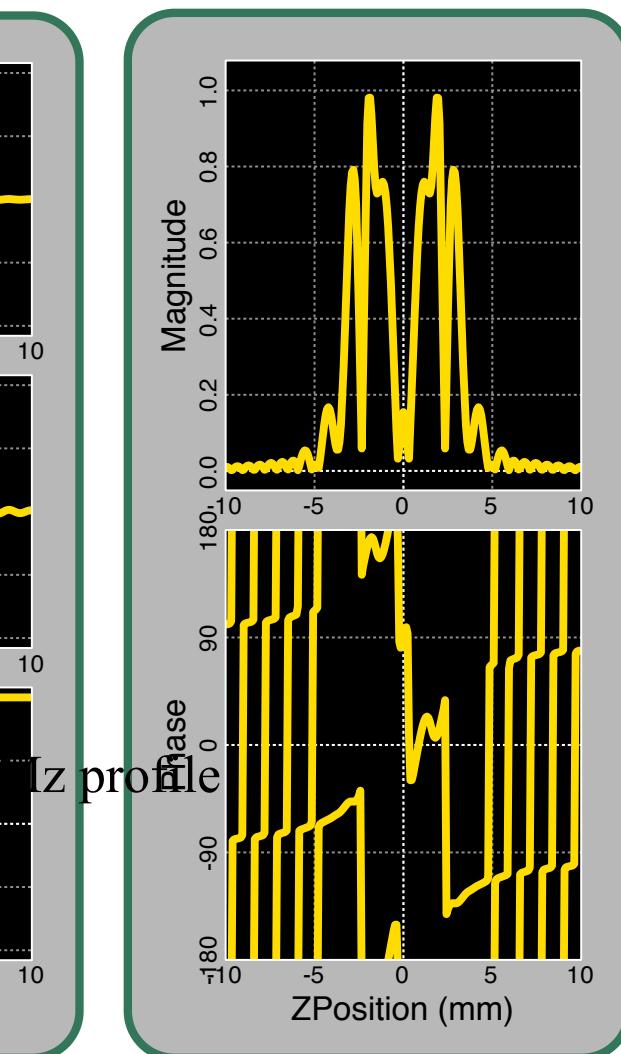
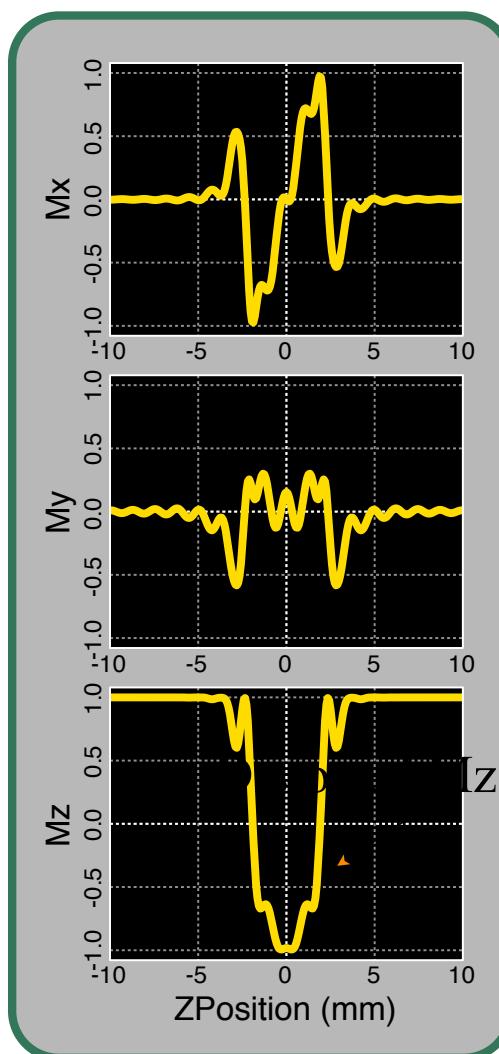
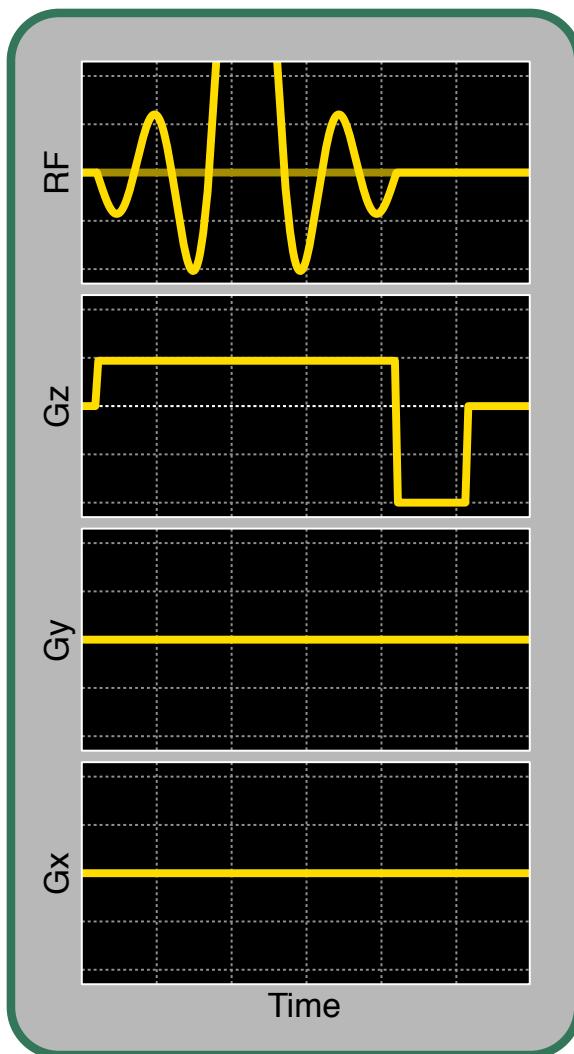
increased  
debands

some phase

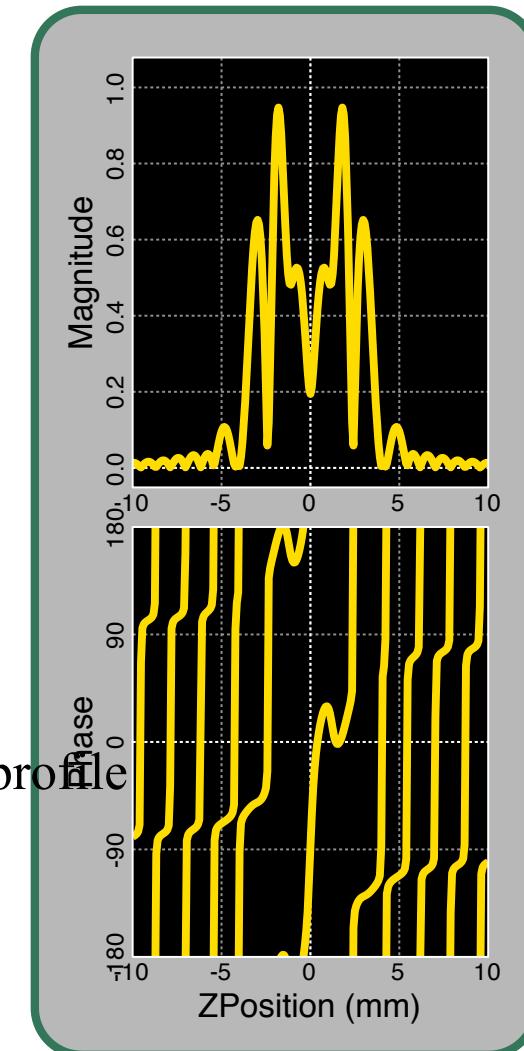
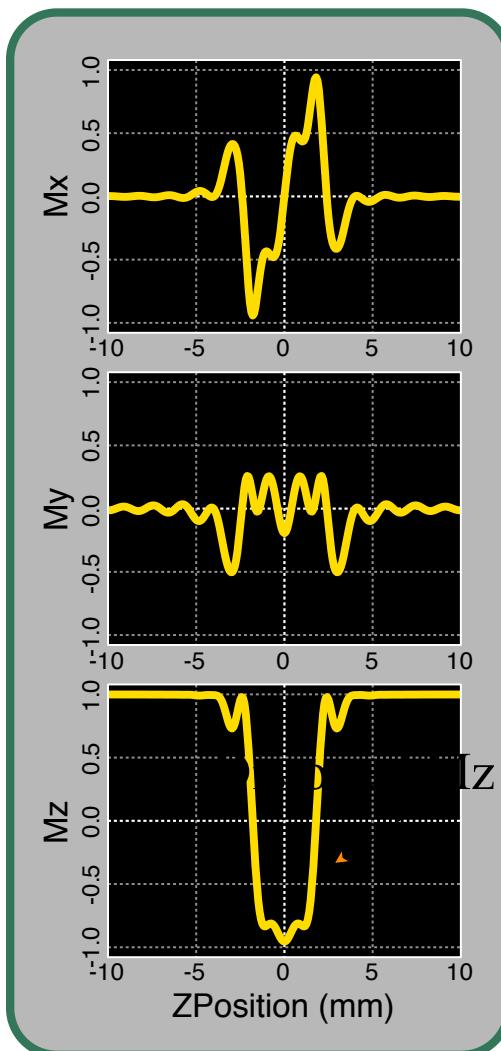
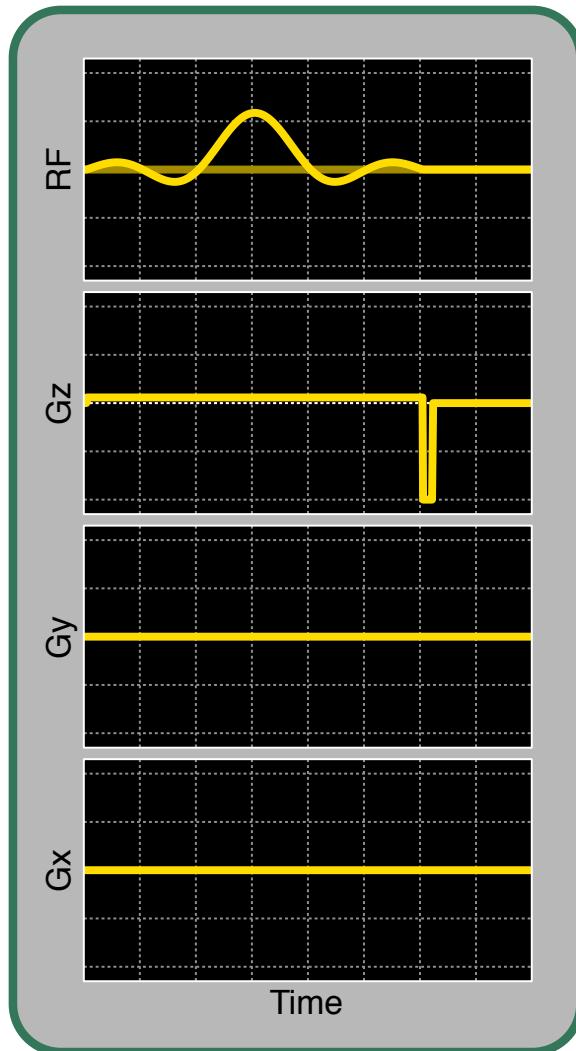
TBW=8, flip = 90, slice = 5mm, duration =2ms



TBW=8, flip = 180, slice = 5mm, duration =2ms



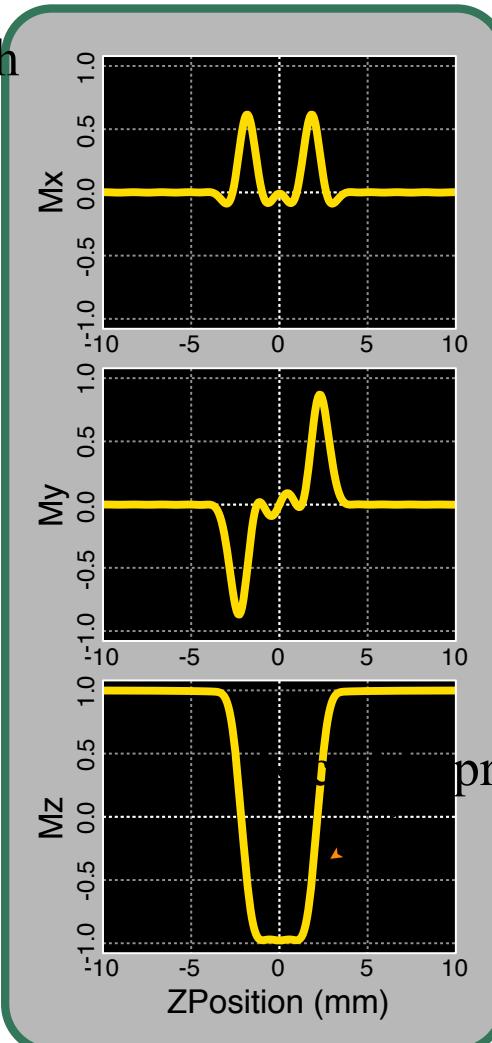
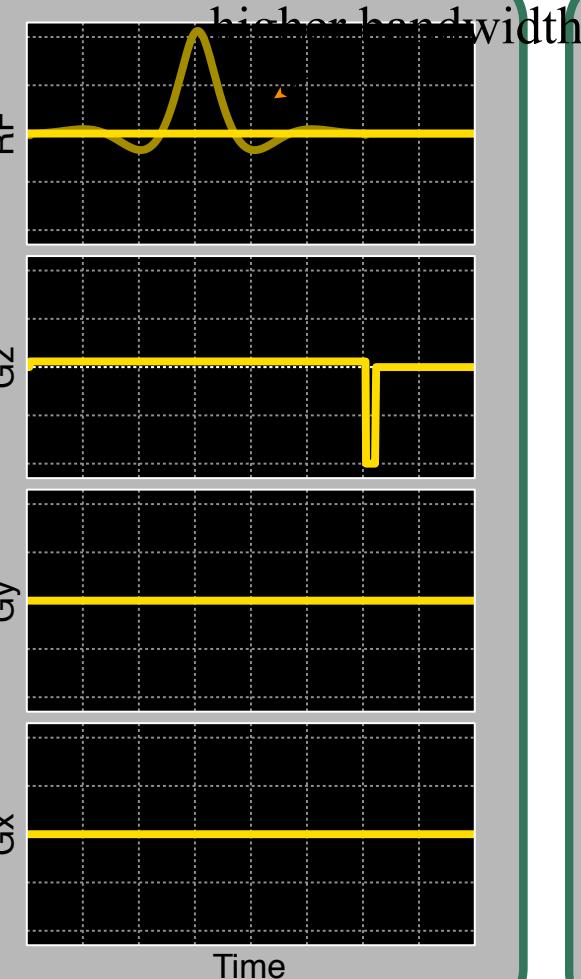
180  
small-tip Pulse



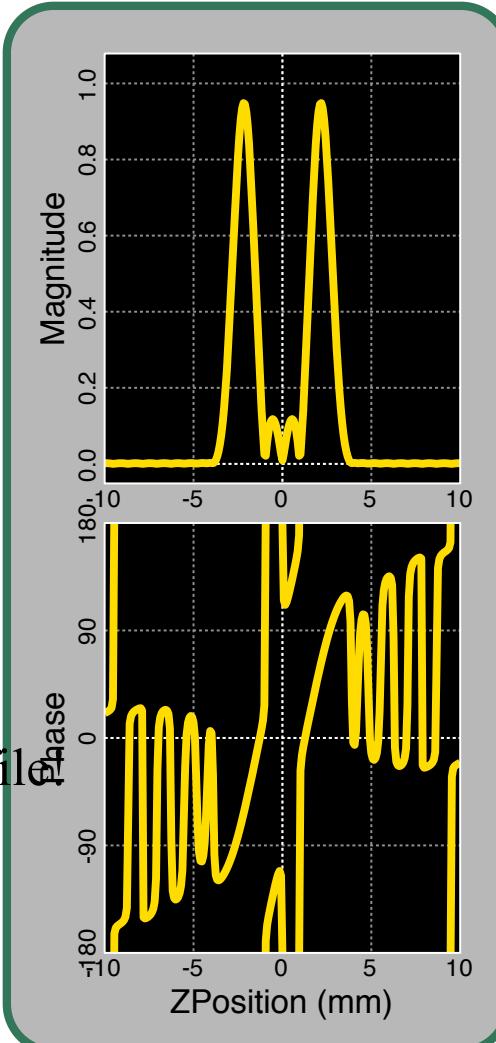
180

## SLR Pulse

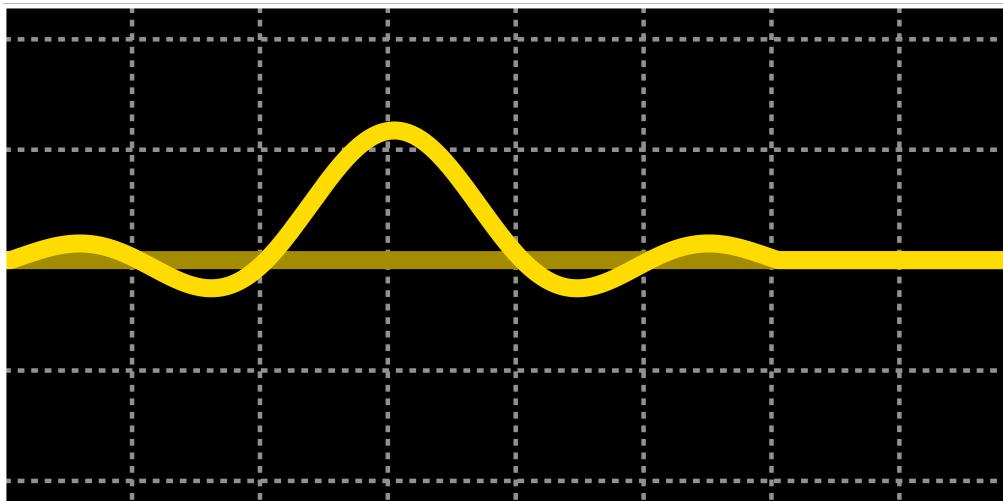
not a sinc!



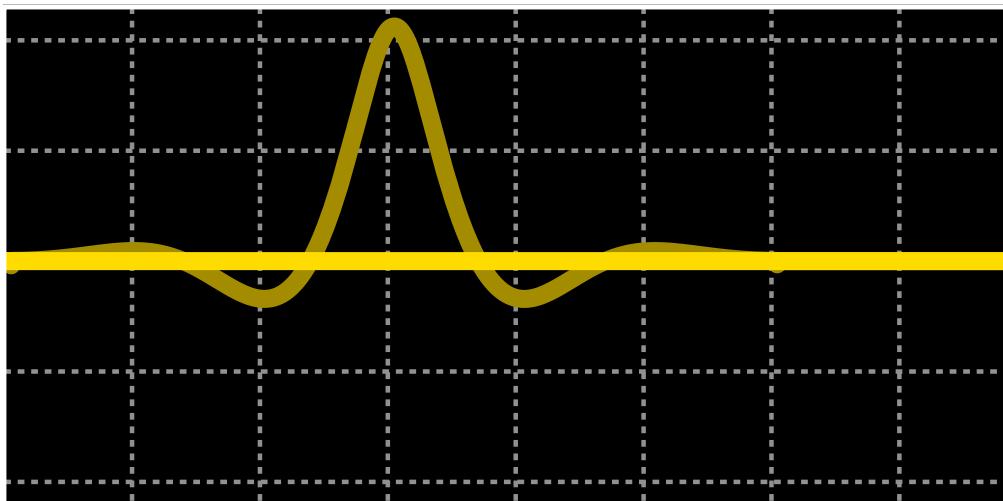
profile



“small-tip” 180



SLR 180



# Spectral-Spatial Pulse

